

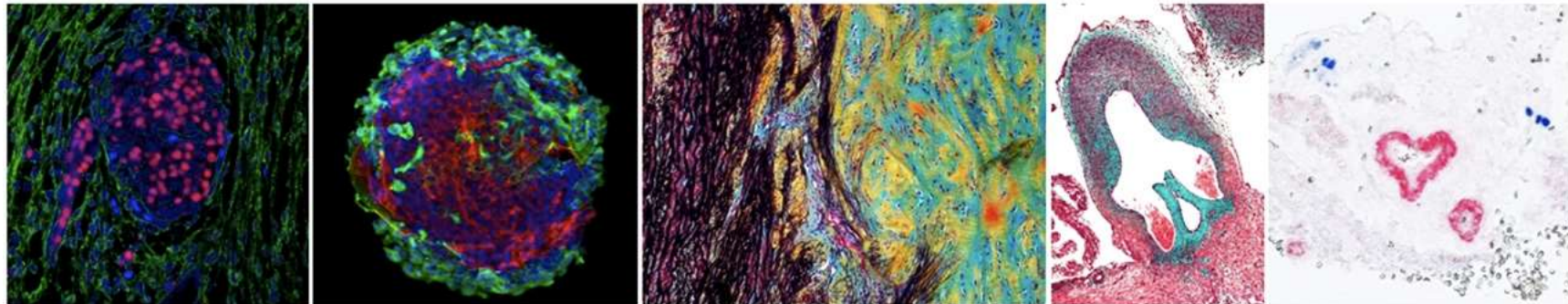
Advanced Microscopy

Eva Brauchle

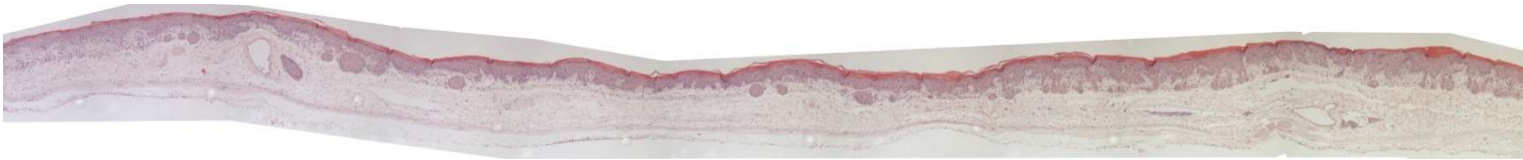
AG Schenke-Layland

Research Institute for Women's Health

University Women's Hospital Tübingen



Advanced Microscopy



Introduction

Basics of light microscopy

Resolution, NA, refractive index, objectives, contrast

Fluorescence Microscopy

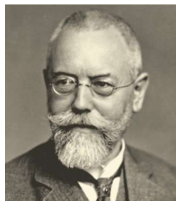
Fluorophores and fluorescence

Wide-field and confocal fluorescence microscopy

Fluorescence Life time imaging microscopy (FLIM)

History of microscopy

Microscope in 1872



$$d = \frac{\lambda}{2n \sin \alpha}$$

Laser scanning microscope, today



History of microscopy

Microscope in 1872



Schott



Abbe



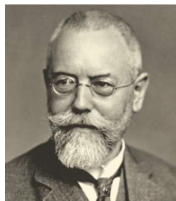
Zeiss



Fraunhofer



Köhler



Zernike



$$d = \frac{\lambda}{2n \sin \alpha}$$

Stokes



Laser scanning microscope, today



Göppert-Mayer



Förster



What does microscopy mean?

- Microscope (from the ancient Greek)

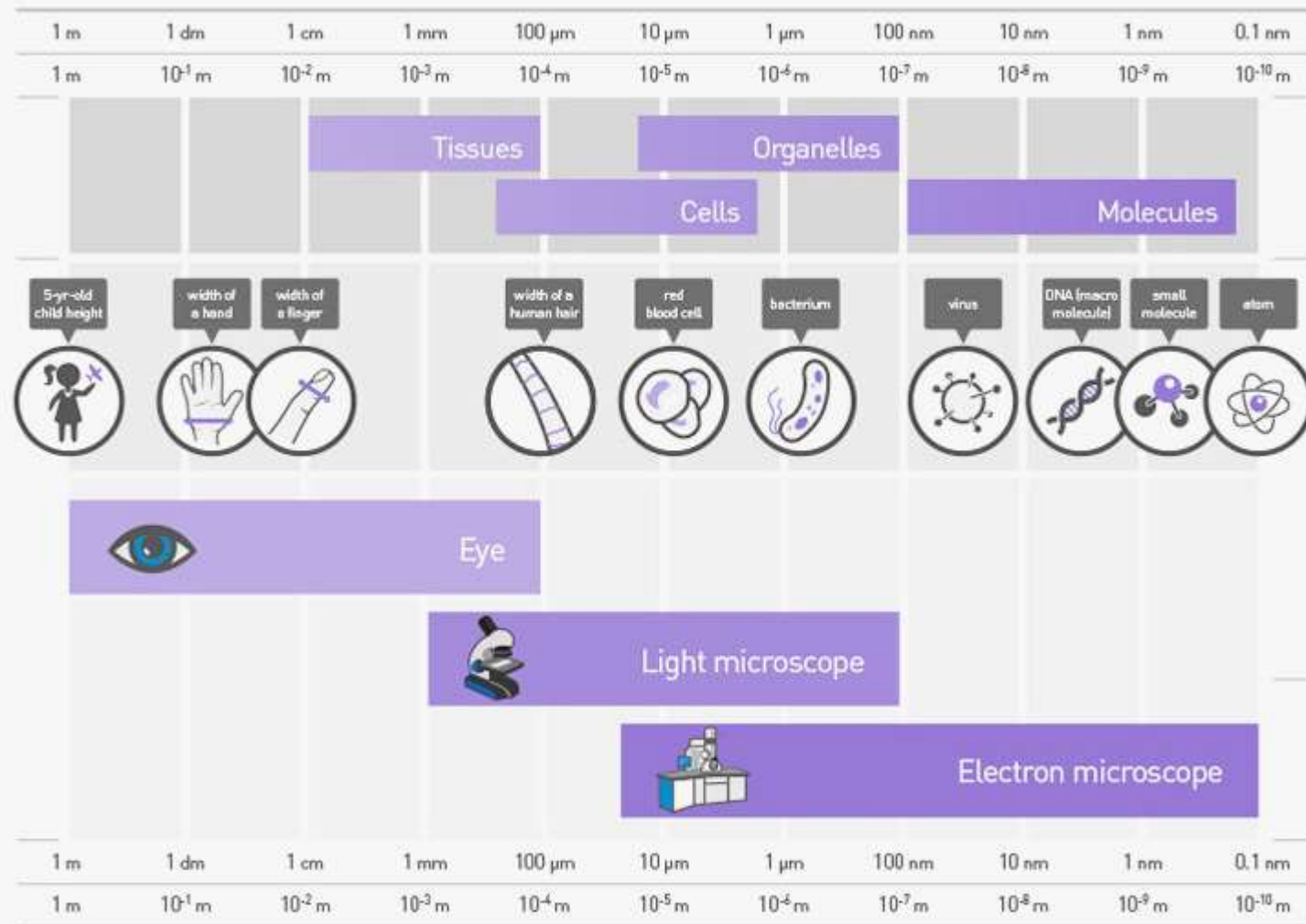
Mikrós = "small"

Skopeîn = "to look" or "see"

- Generating a larger image of something small
- Stepwise and multiple magnification
- Basic principle: objective generates a magnified intermediate image, which is again magnified by the tube lens



Resolving power of microscopes

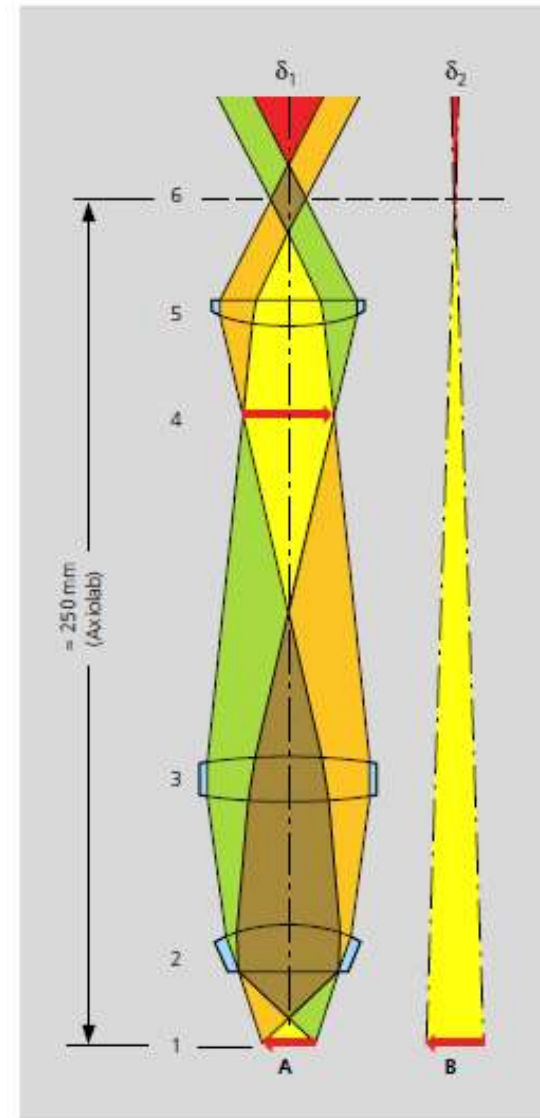


Basic light pathway

1. Object
2. Objective
3. Tube lens
4. Magnified intermediate image
5. Eyepiece (ocular)
6. Eye

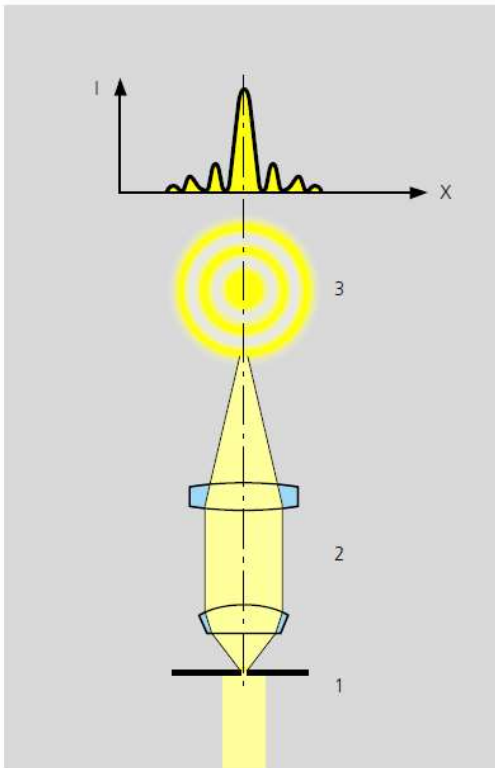
Magnification:

$$M_{\text{microscope}} = M_{\text{objective}} \times M_{\text{ocular}}$$



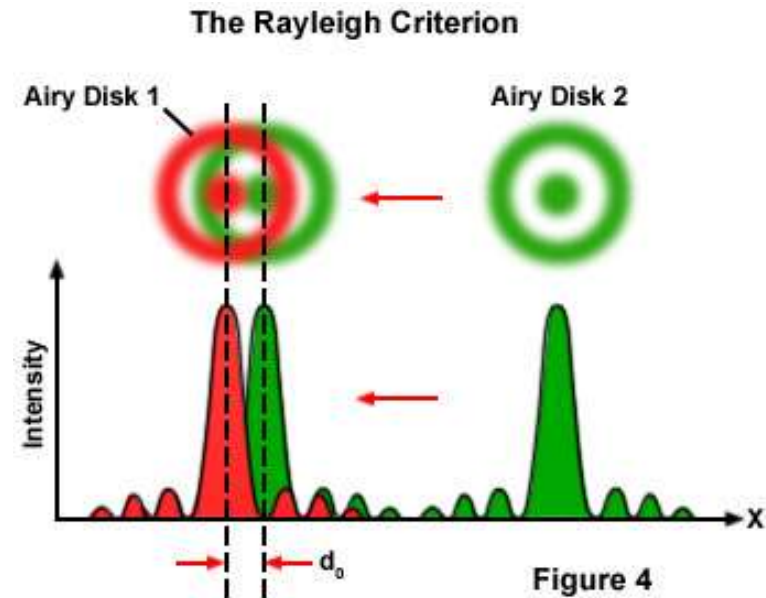
Resolution

- Objective and tube lens image an 'airy disc'



Zeiss: Microscopy from the very beginning

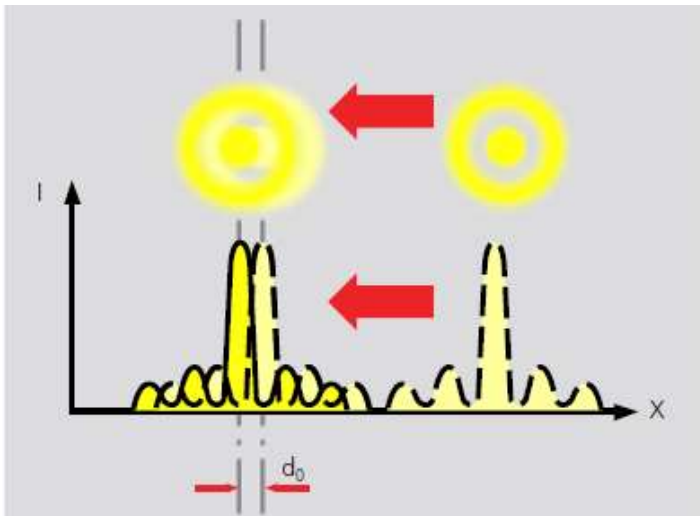
- 1 Object
- 2 Objective and tube lens
- 3 Diffraction rings = "airy disk"



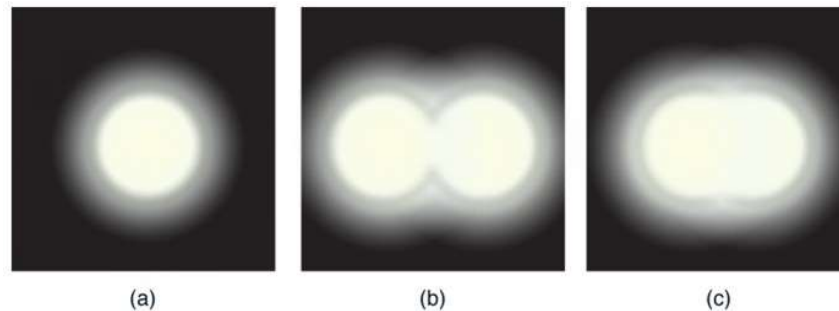
Resolution



- d_0 = distance at which two points are seen separable



Zeiss: Microscopy from the very beginning



<https://courses.lumenlearning.com/austincc-physics2/chapter/27-6-limits-of-resolution-the-rayleigh-criterion/>

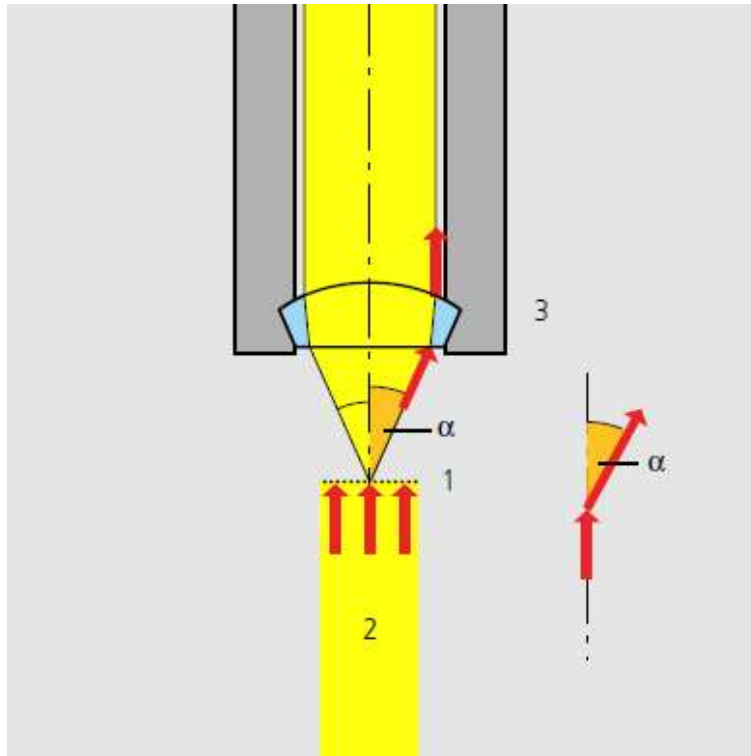
Abbe formula:

$$d_0 = \frac{1.22\lambda}{N.A_{\text{obj.}} + N.A_{\text{Cond}}} \quad \text{or more simply } d_0 = \frac{\lambda}{2N.A.}$$

λ = wavelength of light, e.g. 550 nm (green)

=> The resolution is dependent on the N.A.

Numerical Aperture (N.A.)



Zeiss: Microscopy from the very beginning

- 1 Object
- 2 Incident light
- 3 Objective

- N.A. = “opening” of an objective
- The smaller the object the more light is diffracted
- To collect sharp images from small objects, the objective needs to collect as much diffracted light as possible

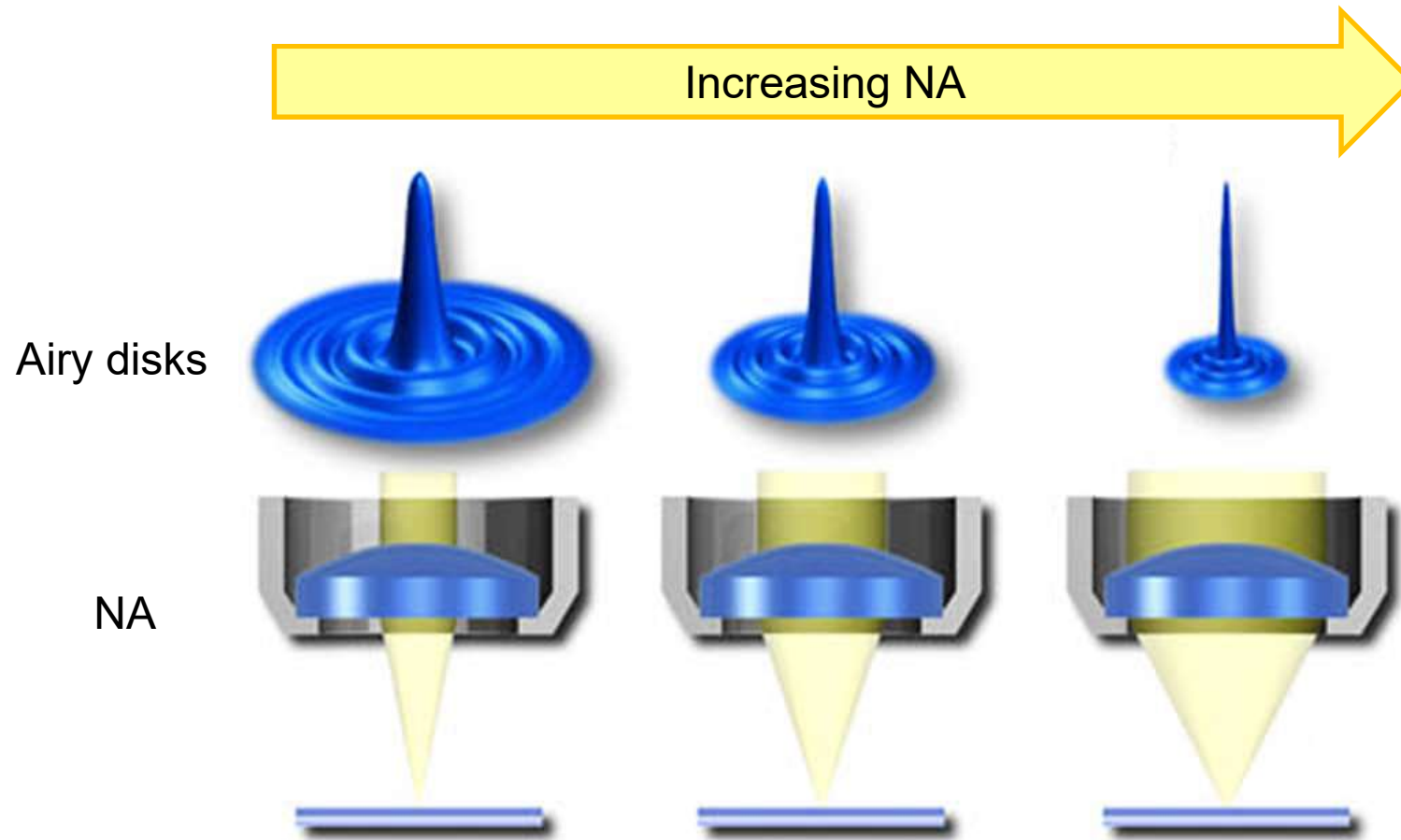
$$\text{Numerical Aperture} = \text{N.A.} = n \cdot \sin \alpha$$

α is half the opening angle of the objective.

n is the refractive index of the immersion medium used between the objective and the object.

($n = 1$ for air; $n = 1.51$ for oil or glass)

Resolution

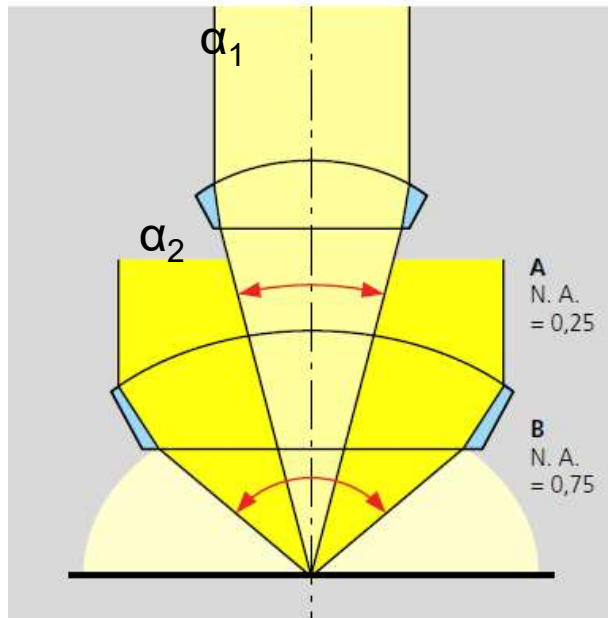


<http://www.olympusmicro.com/primer/anatomy/numaperture.html>

Increasing the resolution

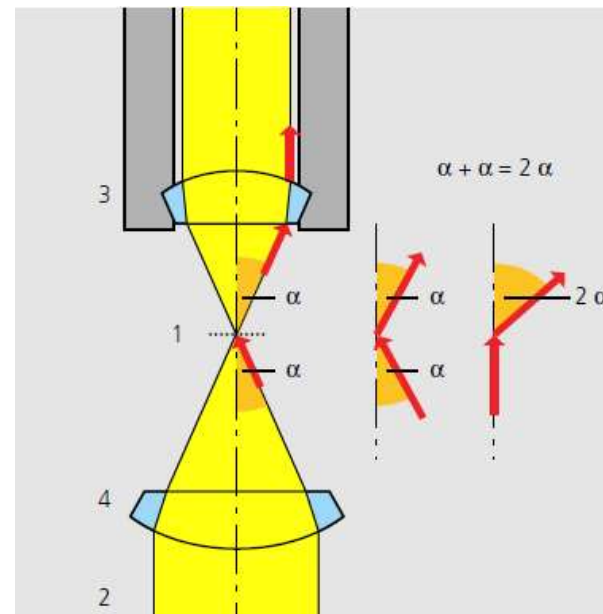
$$d_0 = \frac{\lambda}{2 \text{N.A.}}$$

Increase N.A. of the objective



Zeiss: Microscopy from the very beginning

Condenser lense (4) with the same N.A. as the objective

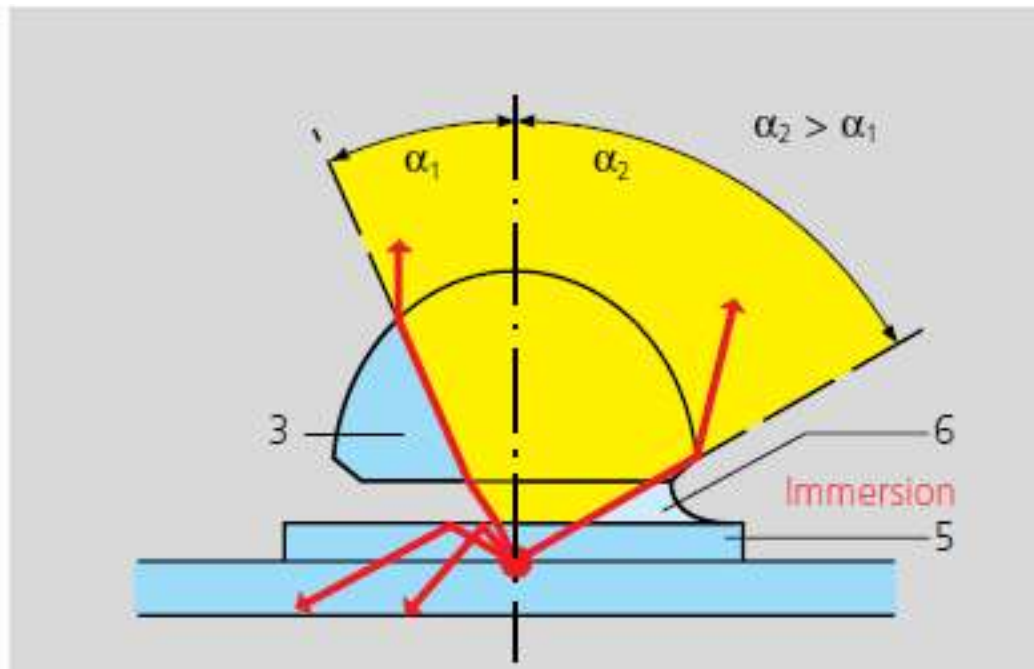


Zeiss: Microscopy from the very beginning

Increasing the resolution

- N.A. is dependent on the refractive index n
- Increasing n due to reduction of the reflections on the microscopic devices

=> more light reaches the objective

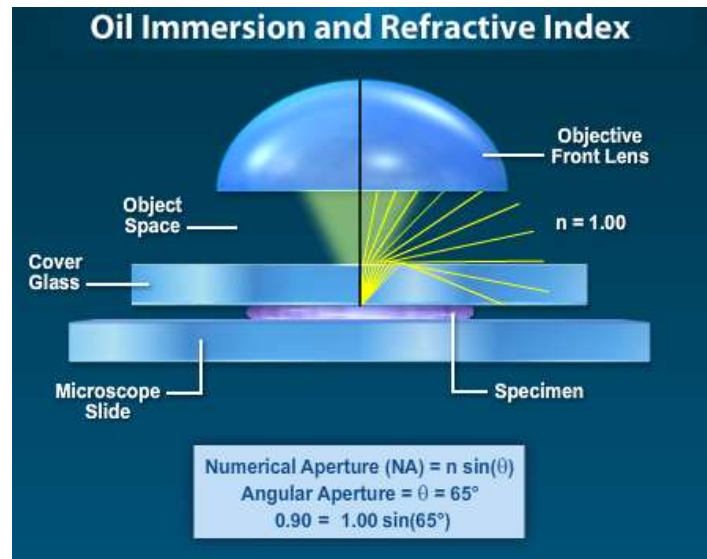


3 Objective
5 Cover slip
6 Immersion liquid

Refractive index

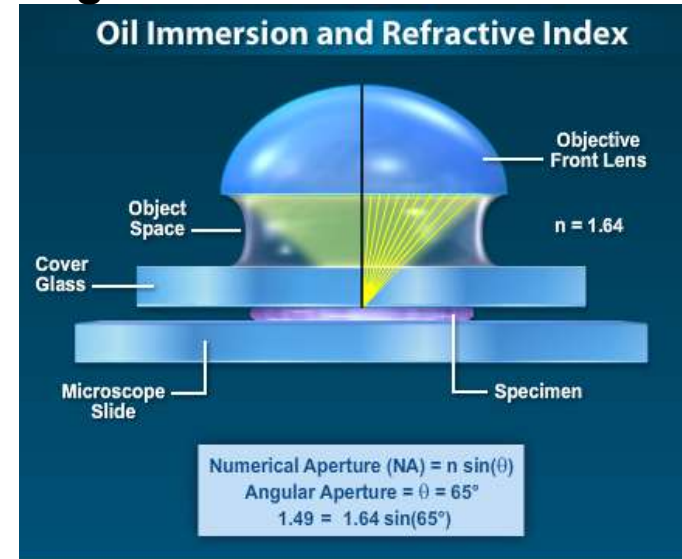
Refractive index n is a value that describes the speed of light in a second medium compared to light speed in vacuum

Low refractive index



<http://zeiss-campus.magnet.fsu.edu/tutorials/basics/oilimmersionrefractiveindex/index.html>

High refractive index



Refractive indices n of immersion liquids

Air	= 1.00
Water	= 1.33
Glycerol	= 1.47
Oil	= 1.57

Objectives



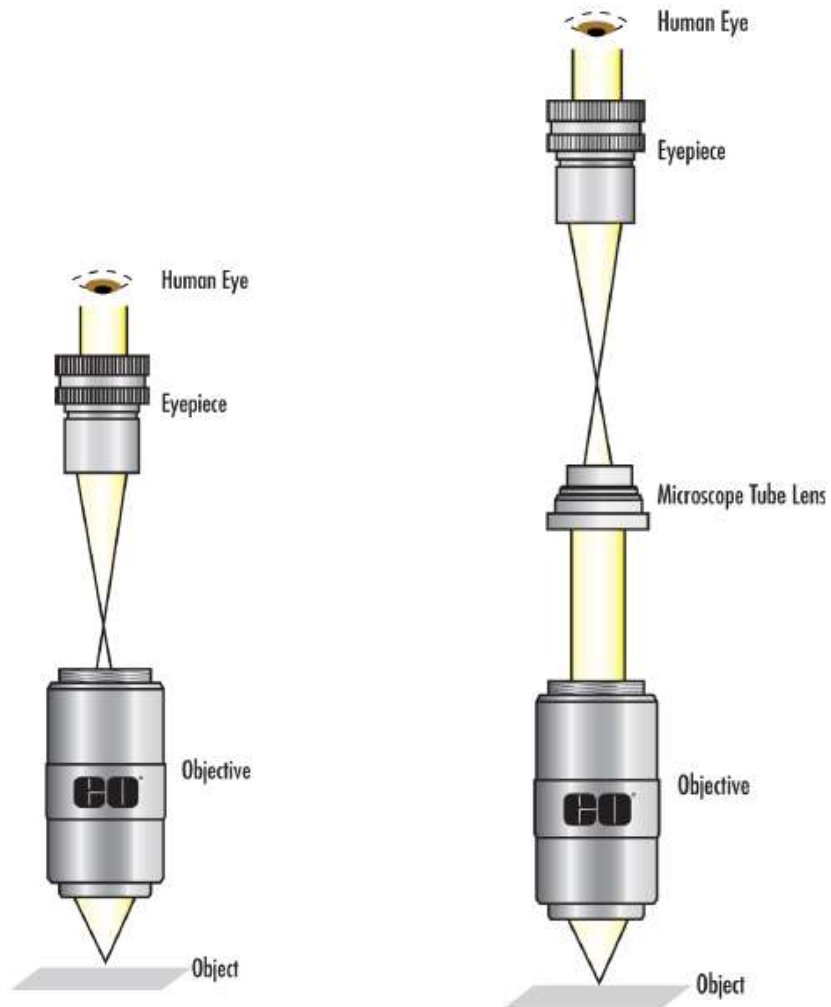
Romeis: Mikroskopische Technik



Magnification	1X	2X	3X	4X	10X	20X	40X	60X	100X
Color Code	Black	Gray	Red	Yellow	Green	Light Blue	Light Blue	Dark Blue	White

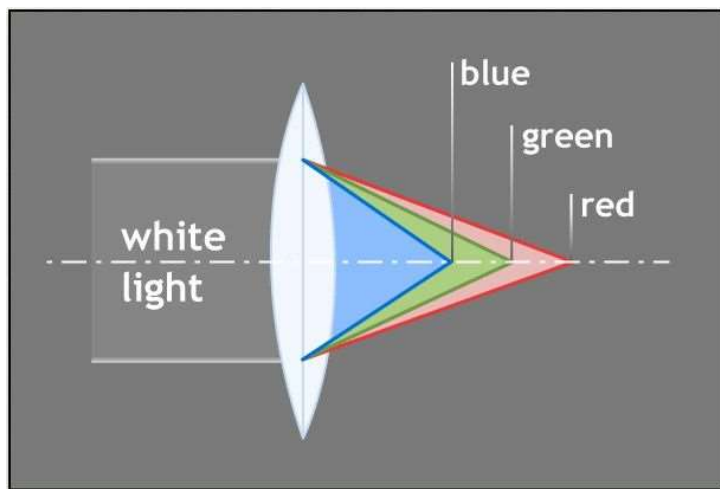
www.edmundoptics.de/technical-resources-center/microscopy/understanding-microscopes-and-objectives/

Infinity-corrected Objectives

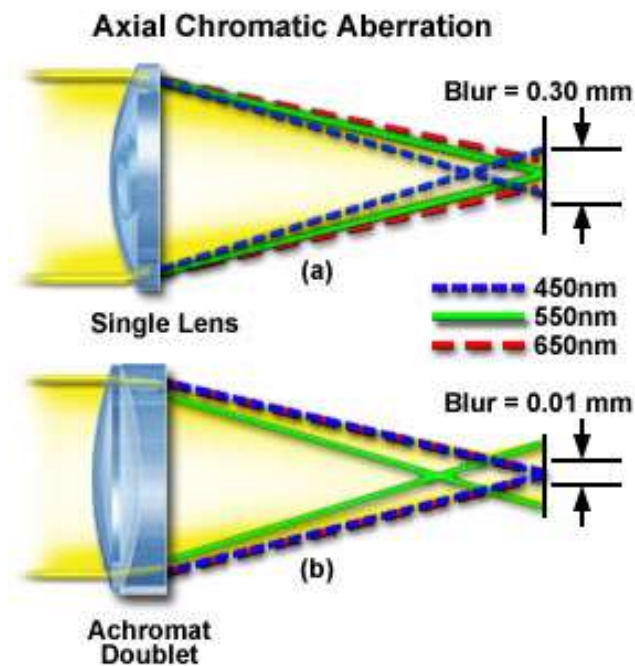


Chromatic aberration

- Failure of the lens to focus all colors on the same point, due to a different refractive index for different light wavelengths
- Achromat is corrected for blue and red light
- Apochromat is additionally corrected for green light



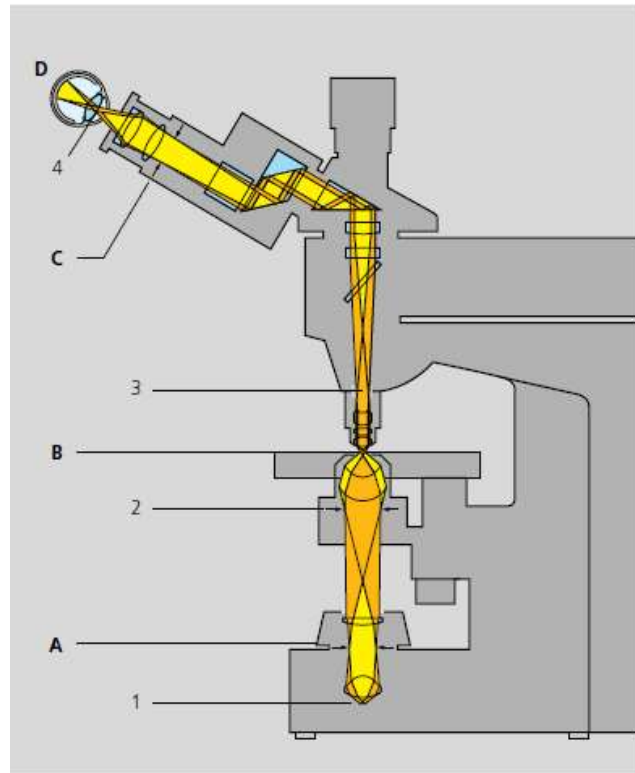
<http://laserpointerforums.com/f54/what-difference-beam-diameter-red-green-blue-lasers-52298.html>



<http://www.microscopyu.com/tutorials/java/aberrations/chromatic/>

Light pathways

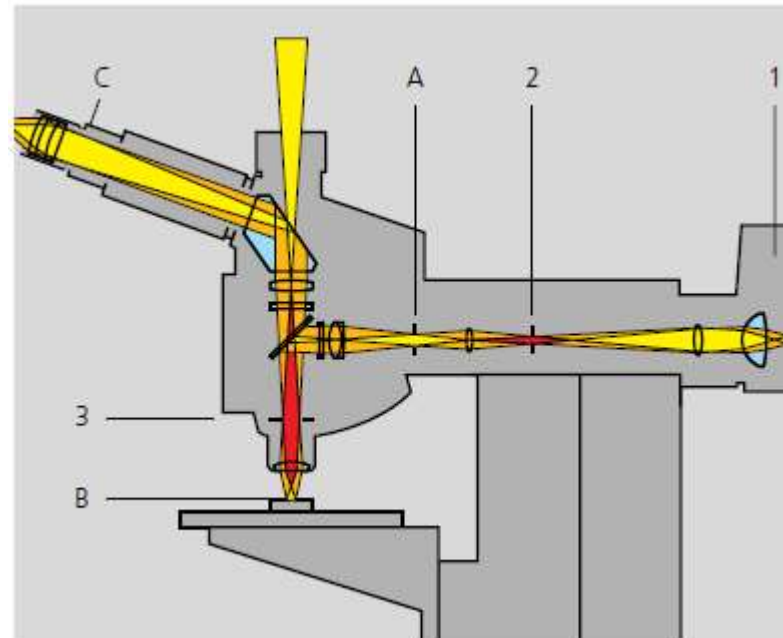
Transmission light microscopy



Zeiss: Microscopy from the very beginning

Two groups of optical planes:

Reflected light microscopy



Zeiss: Microscopy from the very beginning

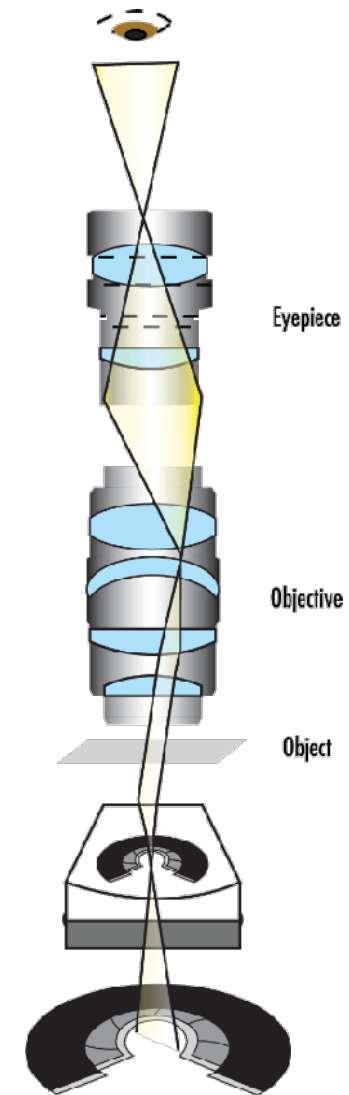
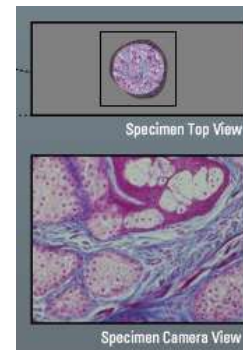
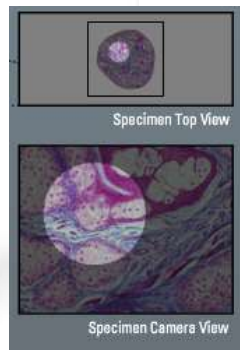
1-4: = beam path of the pupil,
determines the resolution
A-D: = image forming beam path

Image Contrast

- Contrast is the difference between the signal in one pixel and that in another that conveys information about the shape of the specimen or the difference in signal intensity between various parts of an image or between details of interest and “background”
- Various physical and digital “filters” can be used to select specific signals
- Contrast enhancing techniques in optical light microscopy
 - Köhler illumination
 - Phase contrast
 - Differential interference contrast (DIC)
 -

Köhler illumination

The illumination of the object is limited to the observed area



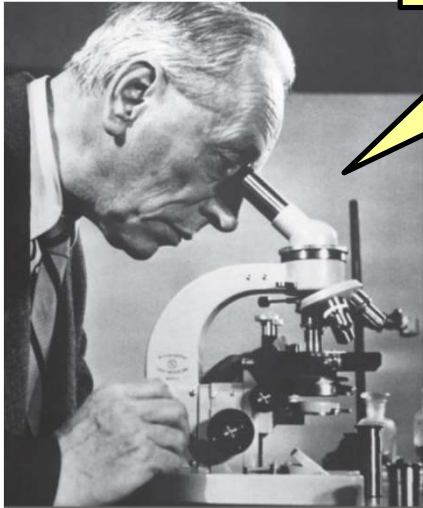
<http://www.leica-microsystems.com/science-lab/koeher-illumination-step-by-step-guide-to-optimal-illumination-of-specimen/>

www.edmundoptics.de/technical-resources-center/microscopy/understanding-microscopes-and-objectives/

Phase contrast

“Phase contrast was not discovered while I was working with a microscope, but originated in my interest in diffraction gratings.”

Dr. Zernike



Murphy: Fundamentals of light microscopy and electronic imaging

bright field

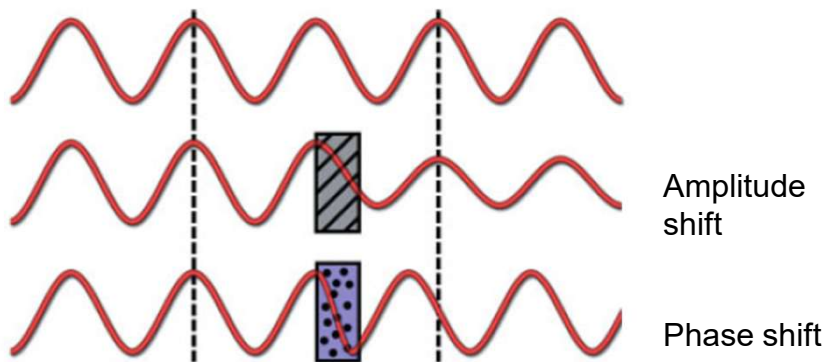


phase contrast

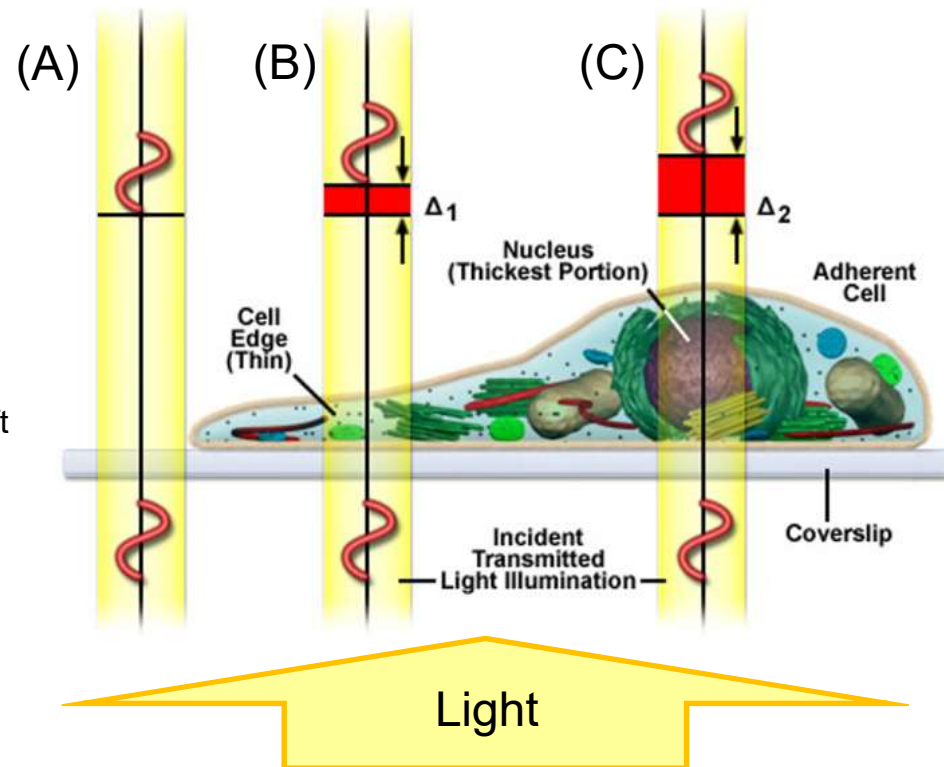


Phase contrast

- Small differences between the refractive indices of the aqueous solution (A) the cell periphery (B) and the nucleus (C)
- Shift of light rays are translated into intensity shifts

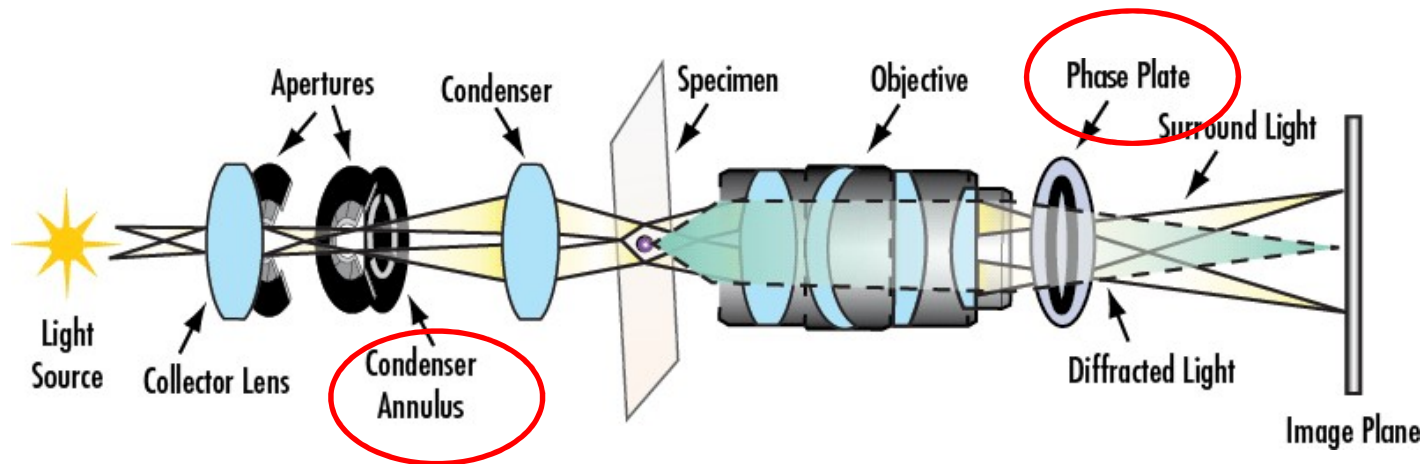


Murphy: Fundamentals of light microscopy and electronic imaging



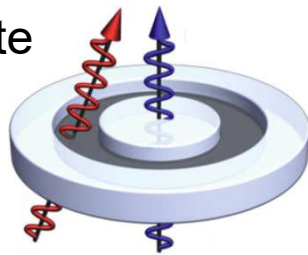
Phase contrast

- Condenser annulus: Opaque plate that illuminates the specimens in defocused parallel light ray
- Phase plate: Alters the phase and amplitude of the light



<http://www.edmundoptics.de/technical-resources-center/microscopy/optical-microscopy-application-phase-contrast/>

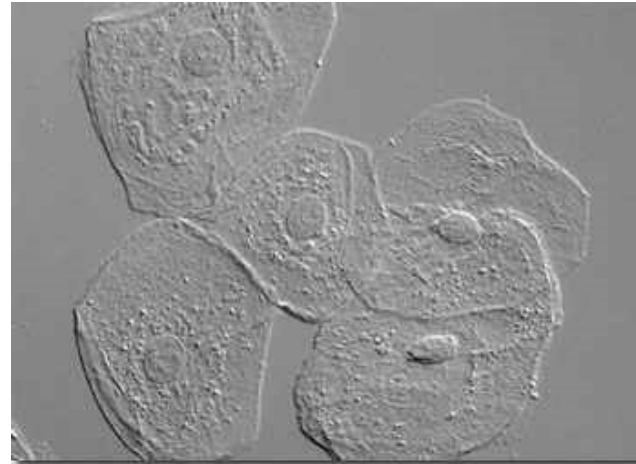
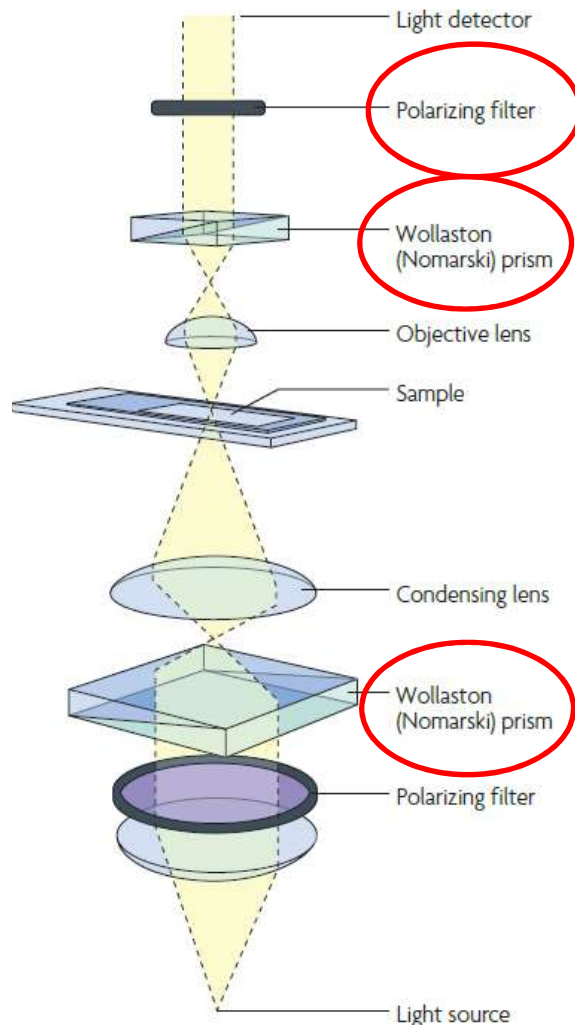
Phase plate



Amplitude of cell-surrounding light is reduced

Murphy: Fundamentals of light microscopy and electronic imaging

Differential interference contrast (DIC)

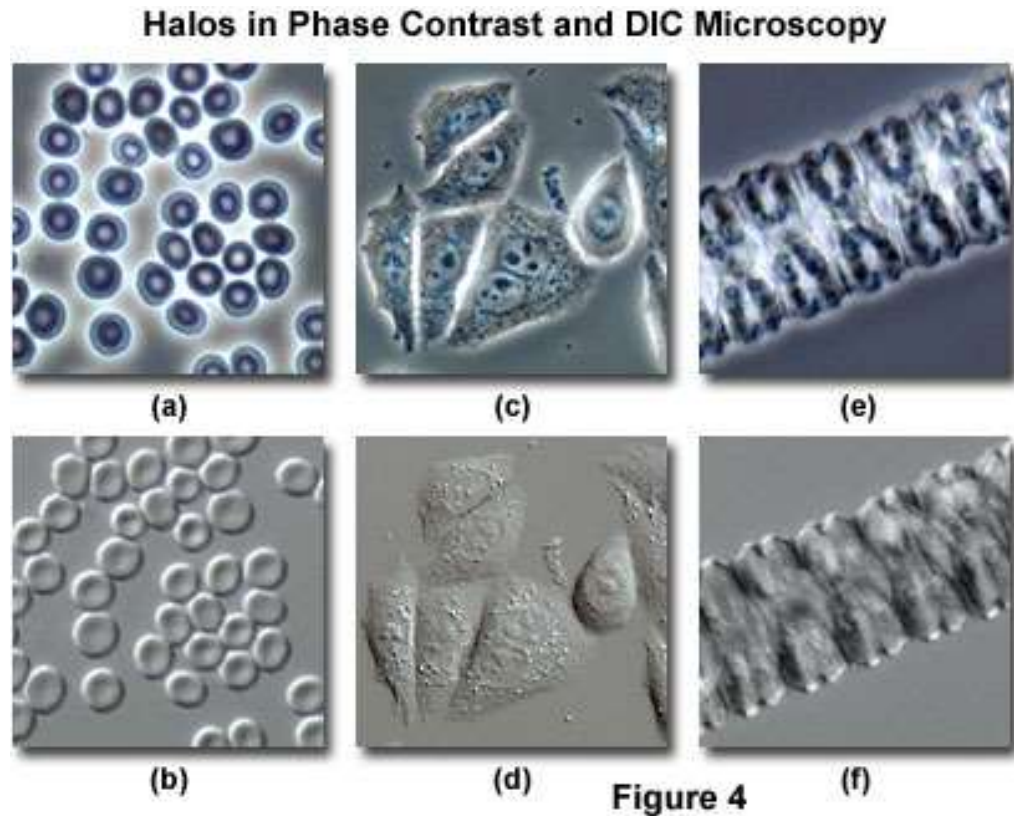


<http://micro.magnet.fsu.edu/primer/techniques/dic/dicgallery/cheekcellsmall.html>

- Use of polarized light
- Wollaston prism separates the light into two sister beams
- Sister beams pass the specimens (phase shifts occurs)
- Second prim fuses the beams and phase shifts were translated into amplitude shift
- Pseudo three-dimensional relief

DIC vs. Phase contrast

- Complementary techniques capable of producing high contrast images of transparent biological phases



Limitations of light microscopy

- Resolution of light microscopy is limited due to the wavelength of the light source and N.A. of objective and condenser
- Optical contrasting methods resolve limited biological information



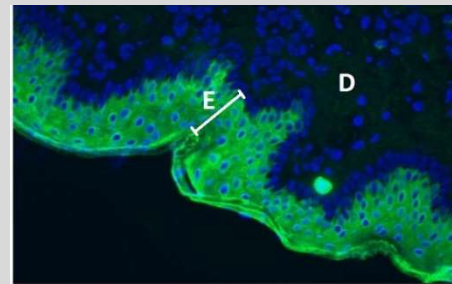
Dyes are needed to visualize specific molecules and structures in biological specimens

Histological dyes

Eosin
Hematoxylin



Fluorescent dyes



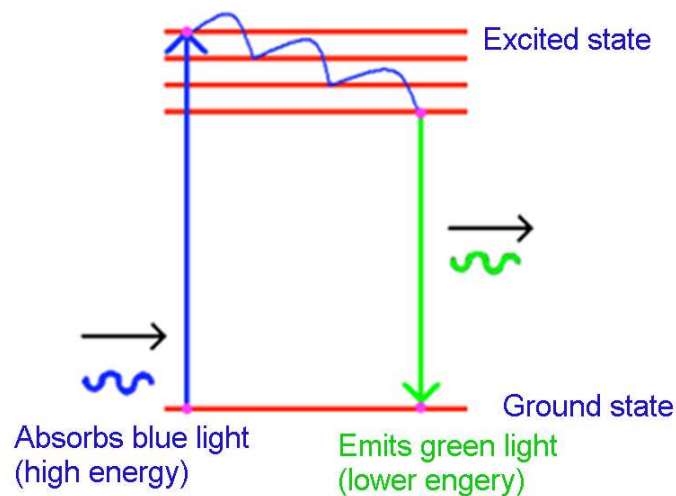
Keratin K10
DAPI

<http://wahoo.nsm.umass.edu/histology/content/fluorescent-image-skin>

Fluorescence Microscopy

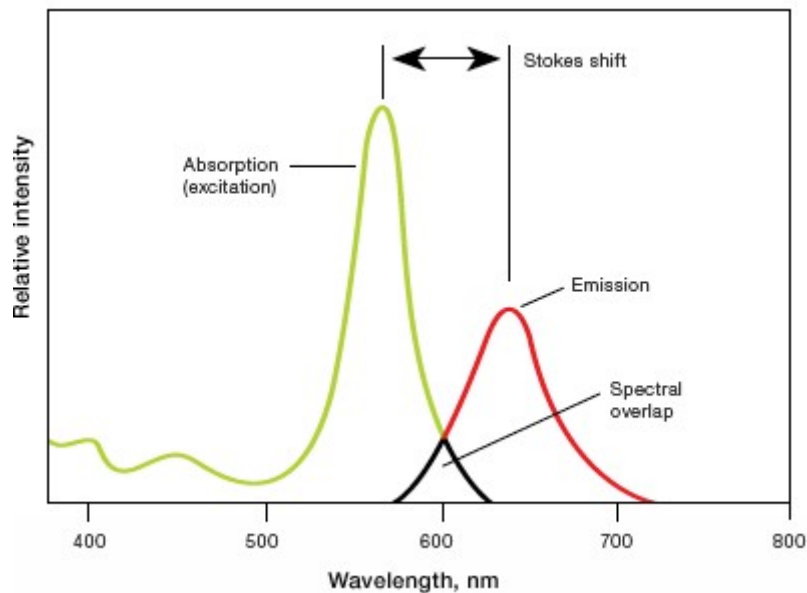
Principle of fluorescence

- Luminescent process in which molecules emit light
- Fluorophores absorb light of one wavelength and emit (fluoresce) light of another wavelength
- Fluorescence light is emitted rapidly during relaxation of excited molecules
- Random process



Principle of fluorescence

- “Stokes shift” describes the wavelength shift from excitation maximum to emission maximum
- “More or less all living samples contain material that is fluorescent by nature, a phenomenon called autofluorescence” (R. Borlinghaus)



Absorption and emission spectrum are specific for a fluorophore

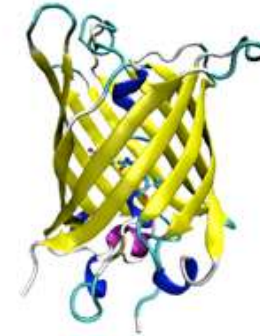
Fluorophores

Fluorescence Intensity F:

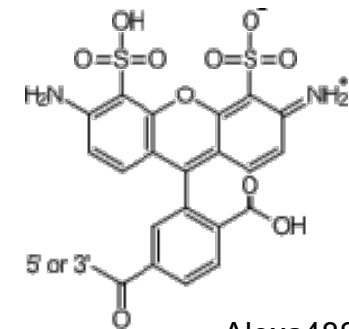
$$F = \sigma * Q * I$$

Q = Quantum yield
I = Excitation light intensity
 σ = Molecular absorption cross section

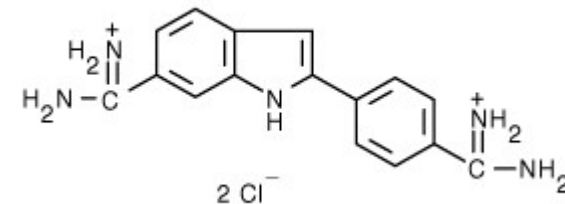
Fluorophore	Quantum yield	λ_{Ex}	λ_{Em}
GFP	0.6	488	535
YFP	0.61	520	542
DsRed	0.79	558	583
Alexa488	0.81	488	535
DAPI	0.58	358	421



Green fluorescent protein (GFP)



Alexa488



4',6-diamidino-2-phenylindole (DAPI)

Fluorophores

Fluorescence life-time

- Every fluorescent molecule has an average time that it spends in the excited state followed after excitation
- Decay of fluorescence intensity after excitation can be measured
- The average time is referred as the fluorescent life time τ

Quenching

- Reversible loss of fluorescence e.g. due to non-radiative energy transfer

Photobleaching

- Irreversible reactions that lead to loss of fluorescence
- Oxygen contributes to photobleaching
- Photobleaching is dependent on molecular environment

Key characteristics of fluorescent probes and specimens

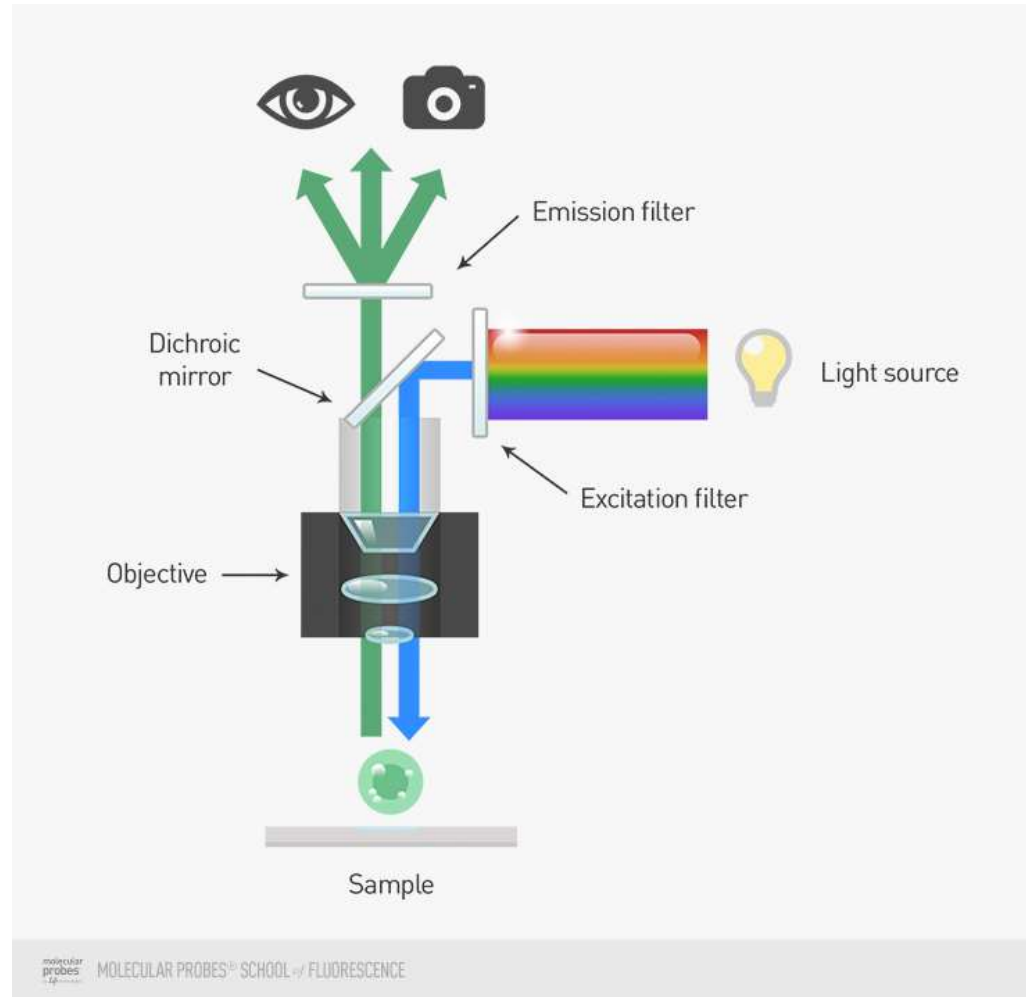
Property	Definition/impact
<i>Optical properties</i>	
Excitation spectrum	Wavelength dependence of the ability of light to induce fluorescence emission of a chromophore
Extinction coefficient ε_λ ($M^{-1} \text{ cm}^{-1}$)	Quantity characterizing a fluorophore's ability to absorb photons at a particular wavelength λ
Emission spectrum	Wavelength dependence of the emitted fluorescence
Fluorescence quantum yield (QY)	Ratio between the number of photons emitted and the number of photons absorbed
Molecular brightness	Product $QY \times \varepsilon$ quantifies the relative rate of photon emission from different fluorophores under identical excitation conditions
Photostability	Resistance to photobleaching, quantified by the quantum yield of photobleaching, that is, ratio of the number of photobleached molecules to the total number of photons absorbed in a sample during the same time interval
<i>Physicochemical properties</i>	
Size	Most often, the smaller the better
Material	May affect chemical stability, toxicity, options to functionalize the probe
Solubility	Most biological applications require aqueous solvents
Cytotoxicity	Effect on sample viability
Phototoxicity	Effect on sample viability
Conjugation chemistry	Determines labeling target
Localization of target	Affects the choice of conjugation
Metabolism of target	Determines temporal stability of labeled construct in live cells

Fluorescent dyes: Examples

Dye	Absorption max [nm]	Emission max [nm]
DAPI	358	461
FITC	495	519
GFP (wildtyp)	395, 475	510
Cy3	547	561
Cy5	647	665
Alexa Fluor 488	495	519
Alexa Fluor 568	578	603
Texas Red	595	615
Rhodamin Red	570	590

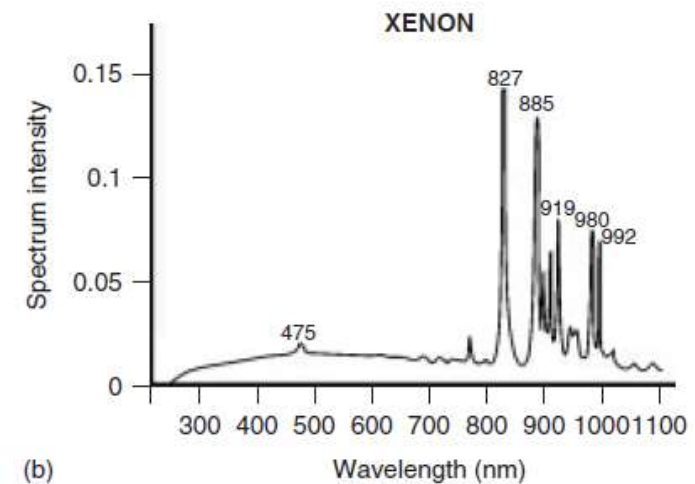
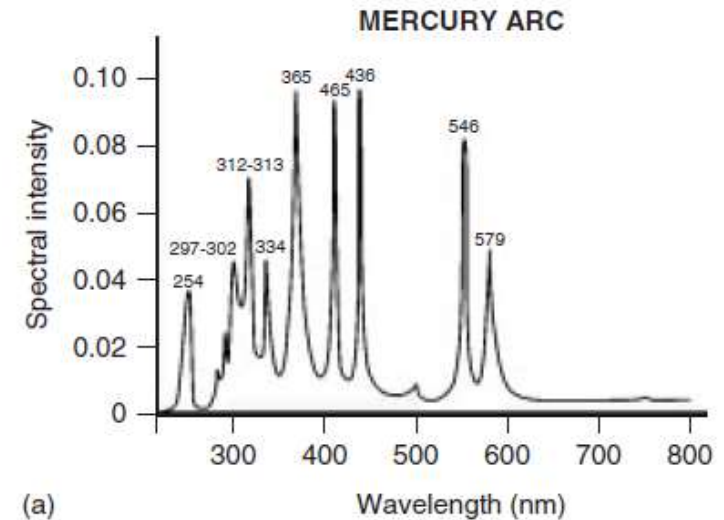
Basic light path: Wide-field fluorescence microscopy

- Dichroic mirror reflects blue (UV) light
- Longer wavelength can pass the mirror



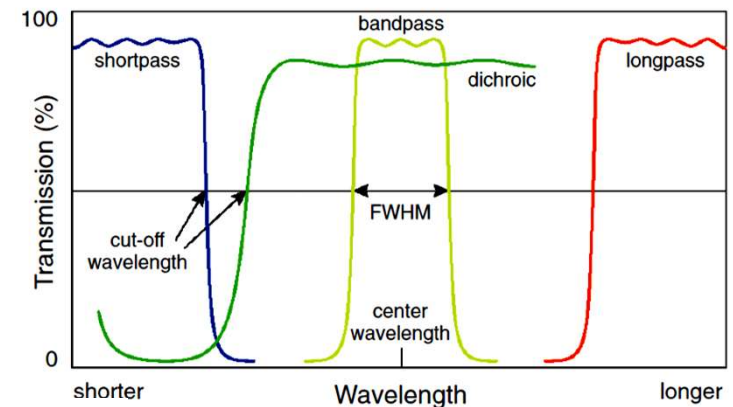
Light sources

- **Broad UV/visible light spectrum**
 - Mercury arc lamp
 - Xenon burner
- **Monochromatic Laser light**
 - Gas lasers
 - Solid state laser
 - Diode lasers

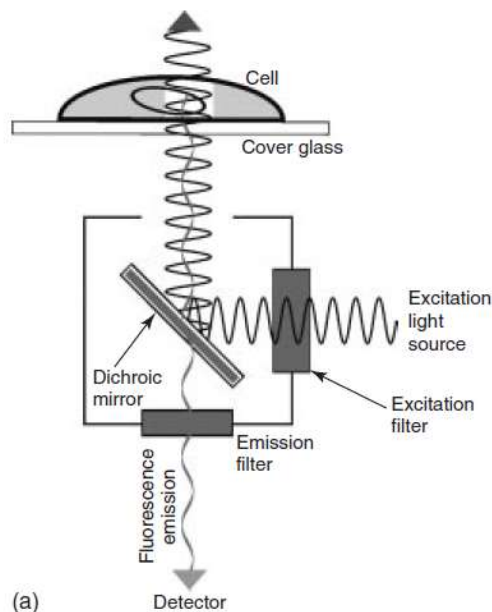


Fluorescence filter units

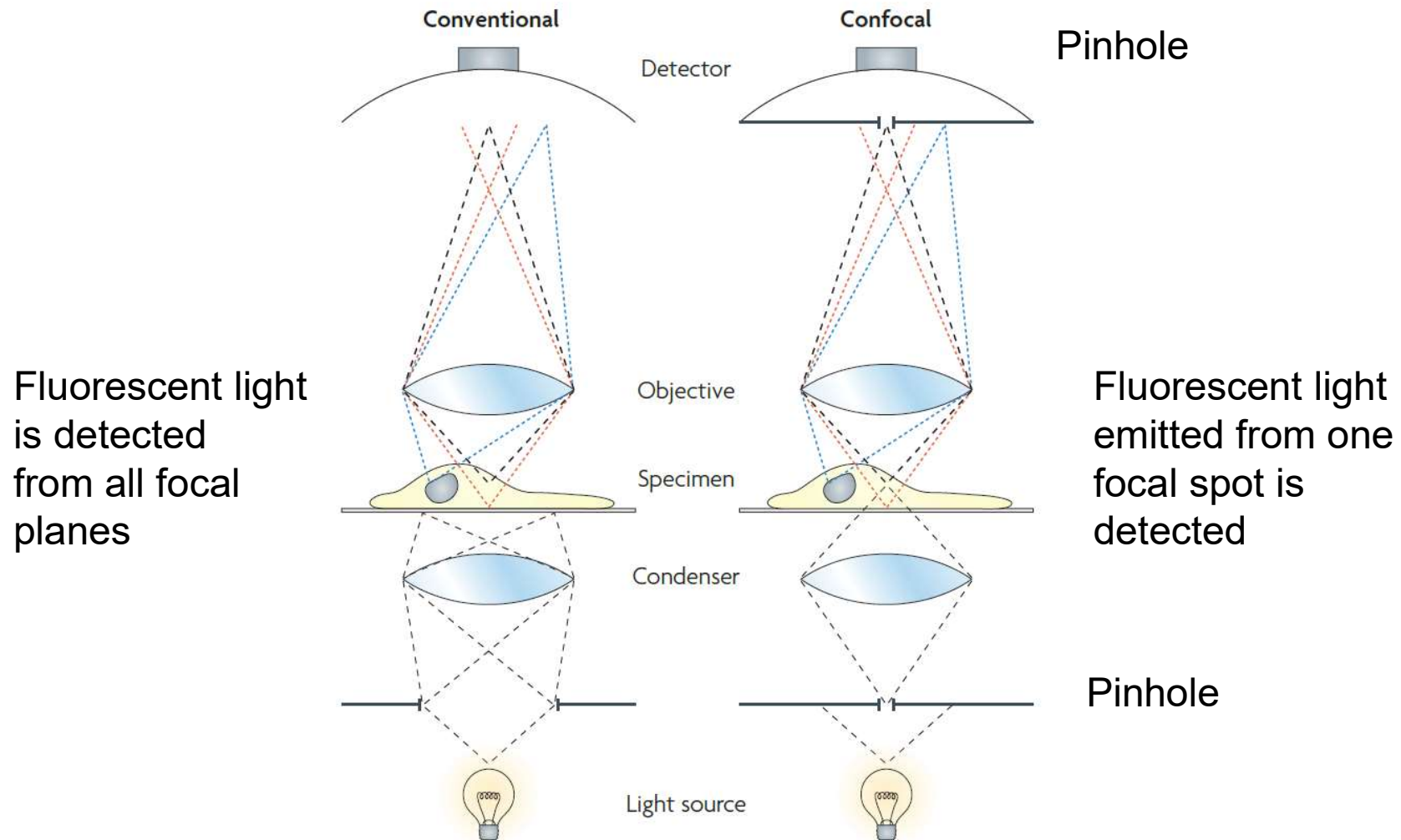
- **Shortpass filter**
Transmits light only below a certain wavelength
- **Bandpass filter**
Transmits light only in a specific segment
- **Longpass filter**
Cuts at defined wavelength



Pawley: Biological confocal microscopy



Set-up of fluorescence microscopes



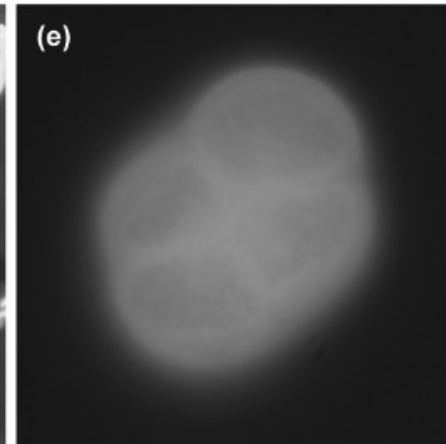
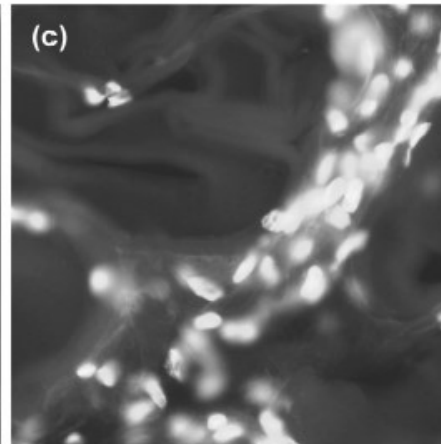
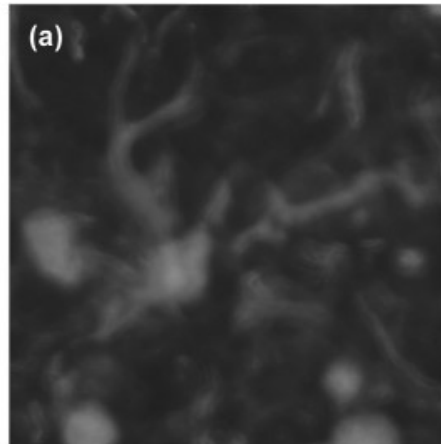
Confocale laser scanning microscopy

Thick section of
mouse hippocampus

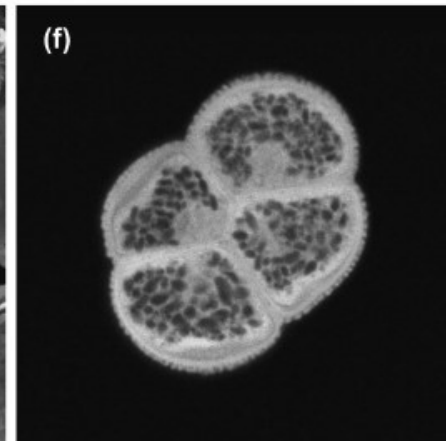
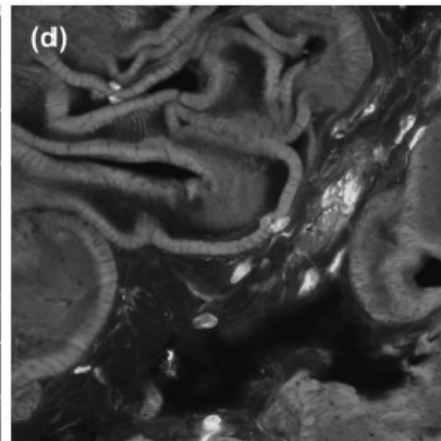
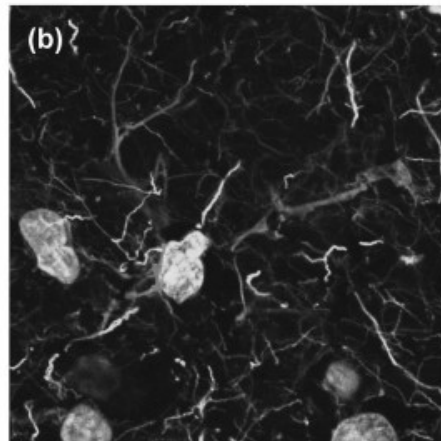
Thick section of
rat smooth muscle

Autofluorescence
of pollen grain

Widefield
microscopy

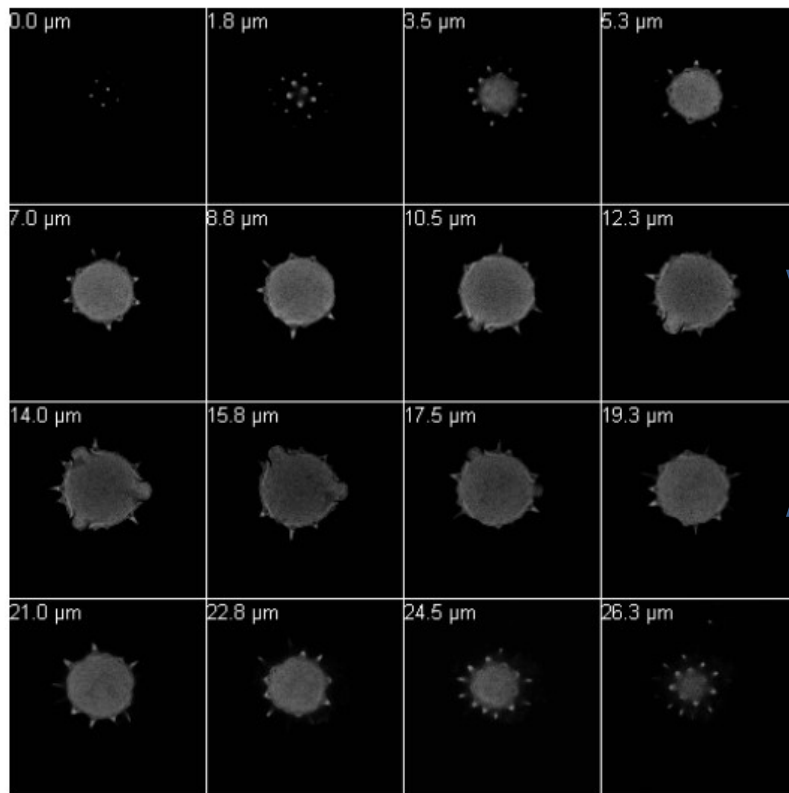


Confocal laser
scanning

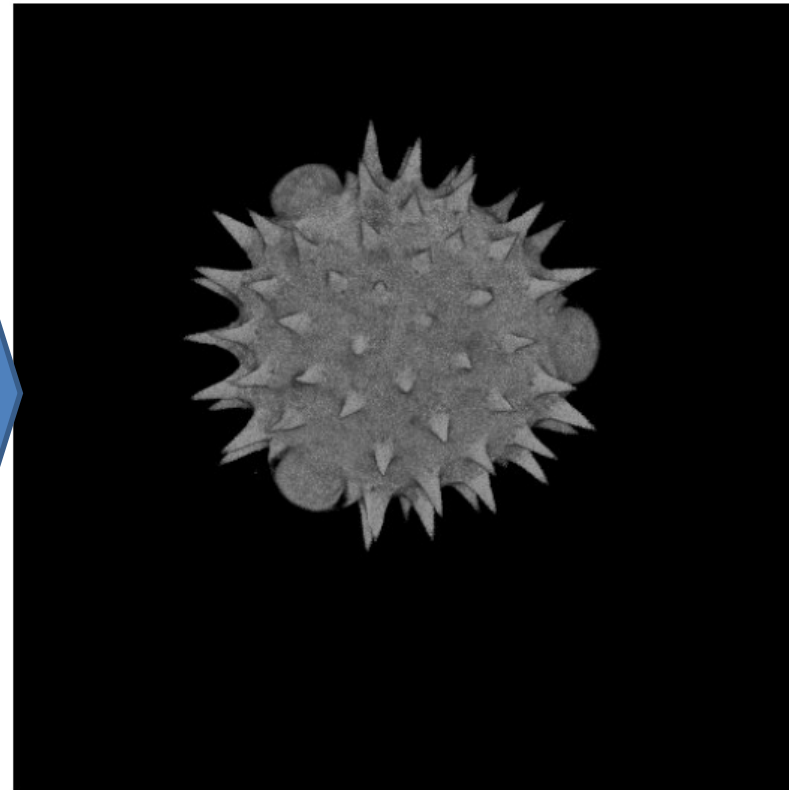


Confocal laser scanning microscopy

Single stacks with variations in z-direction



3D Projection

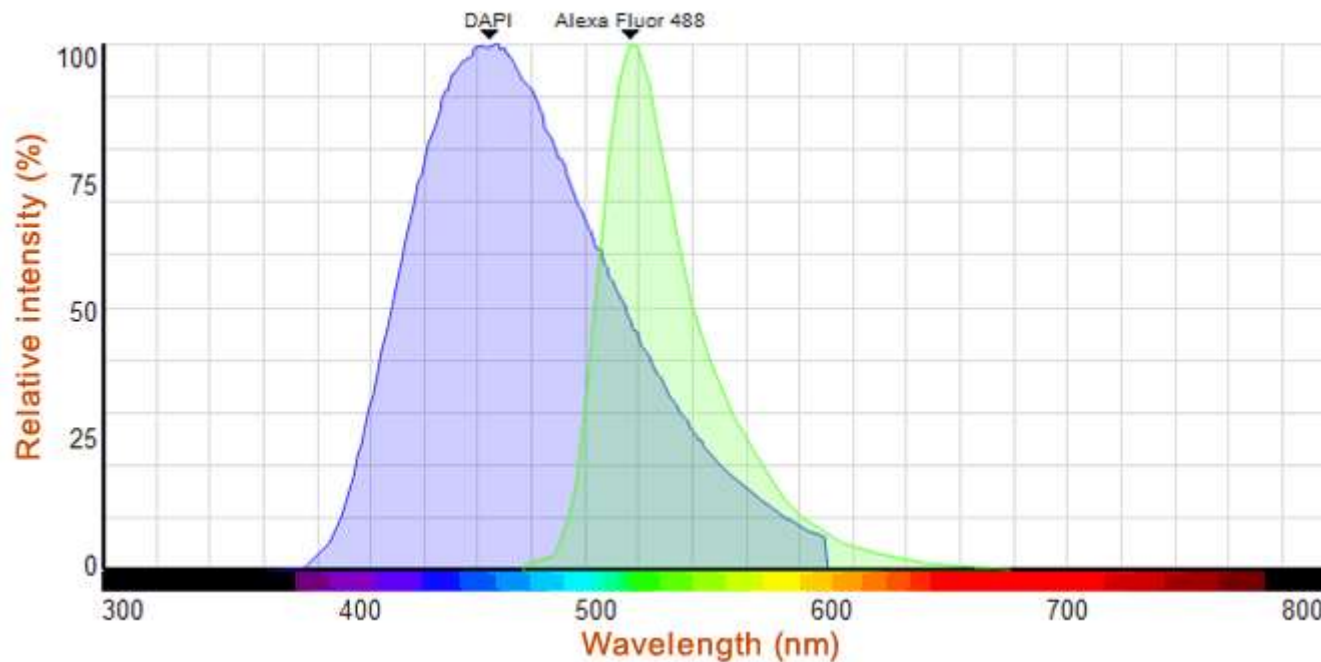


Zeiss brochure: Confocal laser scanning microscopy

Simultaneous Fluorescence Imaging

- When two (or more) fluorescent probes are used within the same sample, it is possible that the emission spectra of the two probes overlap

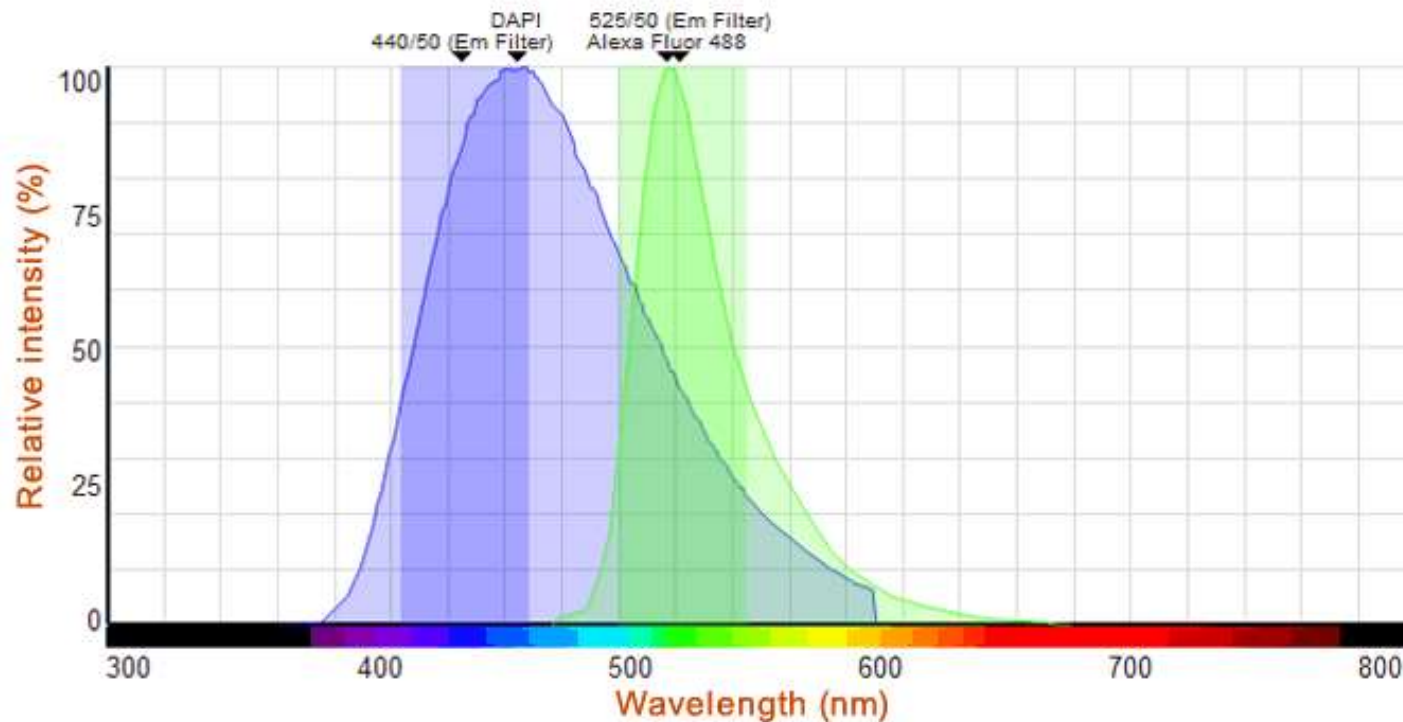
Emission spectra for DAPI (blue) and AF488 (green)



<http://www.ammrf.org.au/myscope/confocal/confocal/image/seqsim/>

Simultaneous Fluorescence Imaging

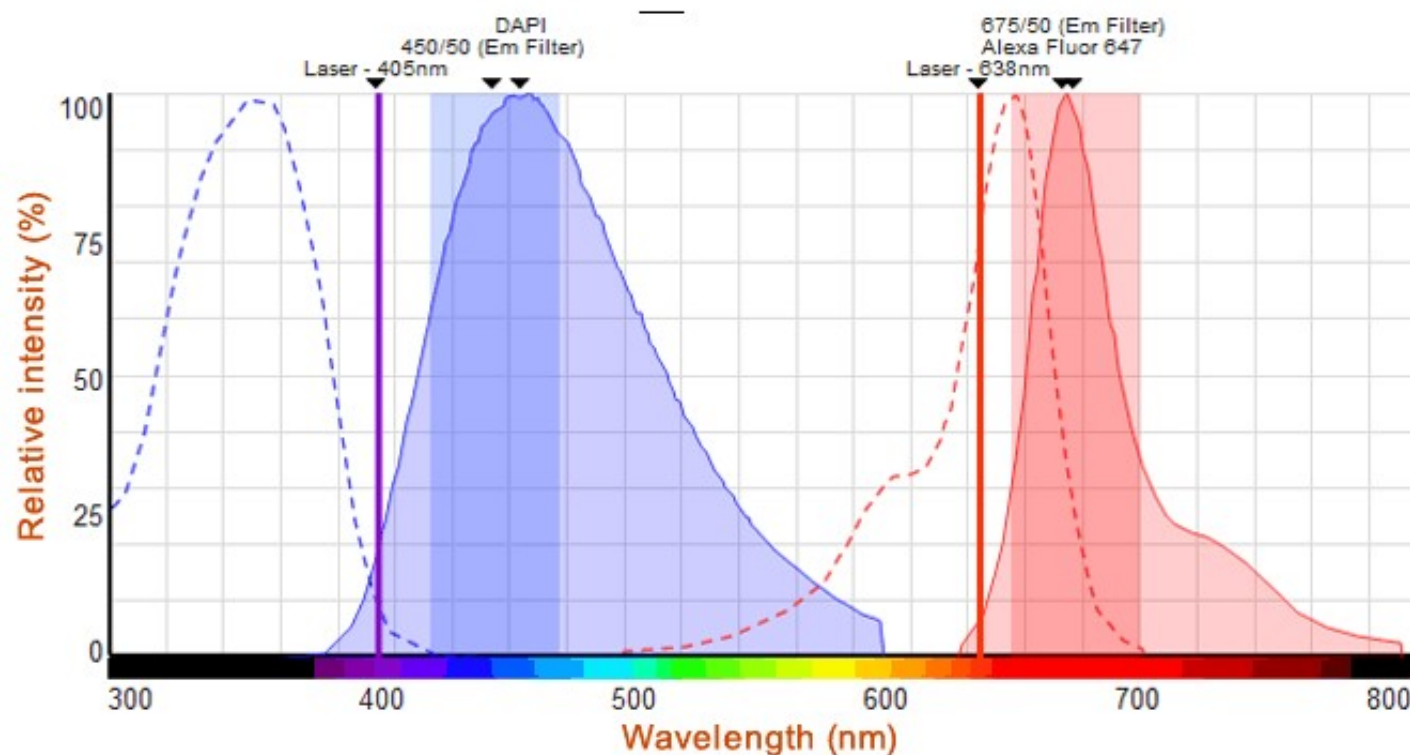
- Some of the fluorescence emission from both DAPI and AF488 will pass through the 525/50nm filter
- About 30% of the total signal detected in the second detector will originate from DAPI



<http://www.ammrf.org.au/myscope/confocal/confocal/image/seqsim/>

Simultaneous Fluorescence Imaging

- Simultaneous imaging of DAPI and AF647
- Minimal cross-excitation or emission of the two fluorophores
- No spectral bleedthrough

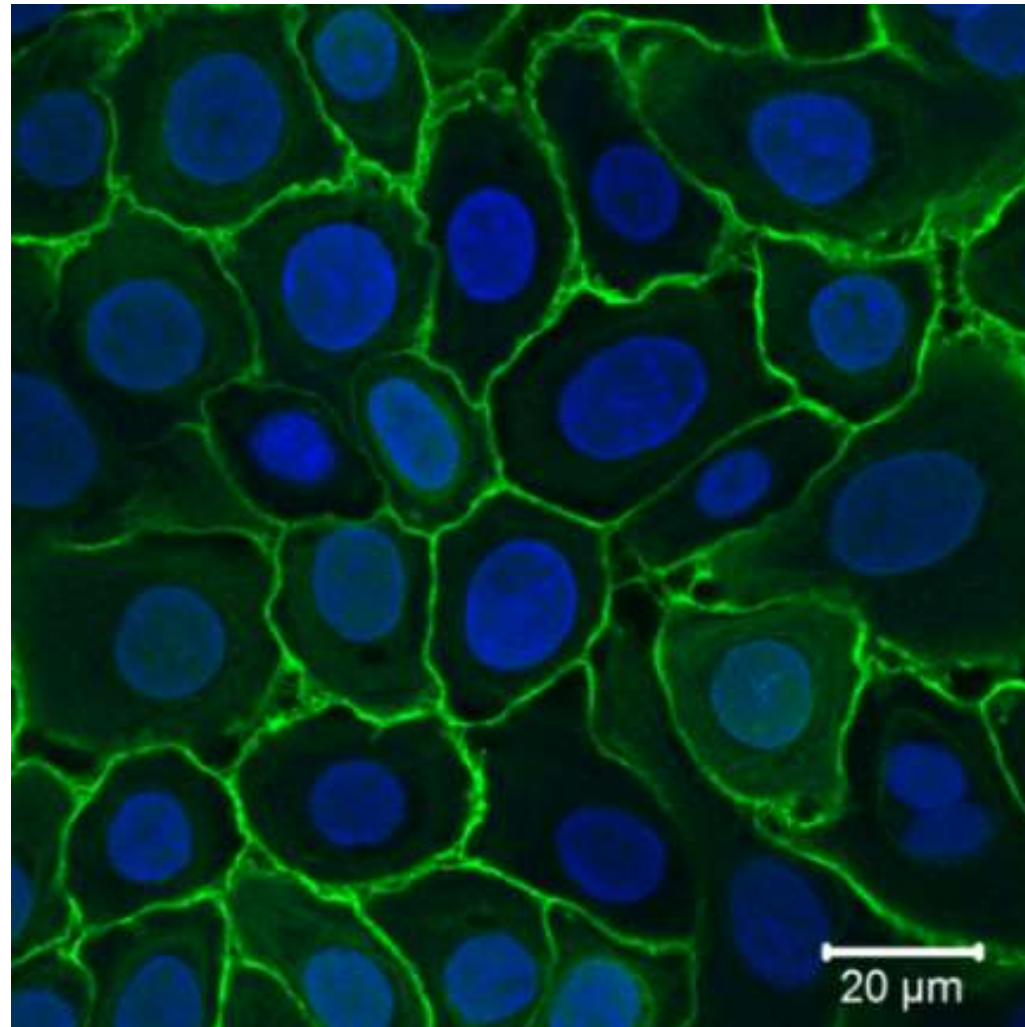


How to get fluorescence into the specimens?

- Fluorescent dyes bind to specific cellular structures (nuclei, mitochondria)
- Antibodies conjugated to fluorophores
- Cells / animals are genetically modified to express fluorescent proteins e.g. green fluorescent protein (GFP)
- Use of intrinsic fluorescence (autofluorescence and multiphoton imaging)

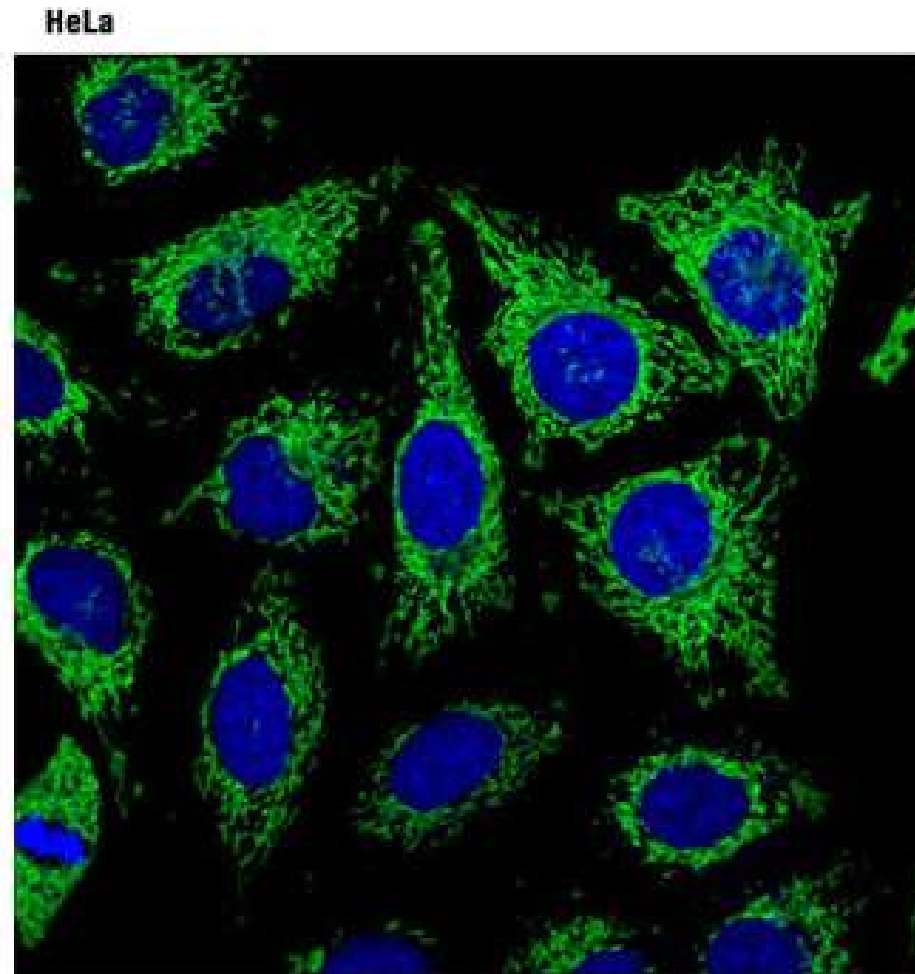
Fluorescent dyes bind to specific cellular structures

- DAPI
- Cell membrane



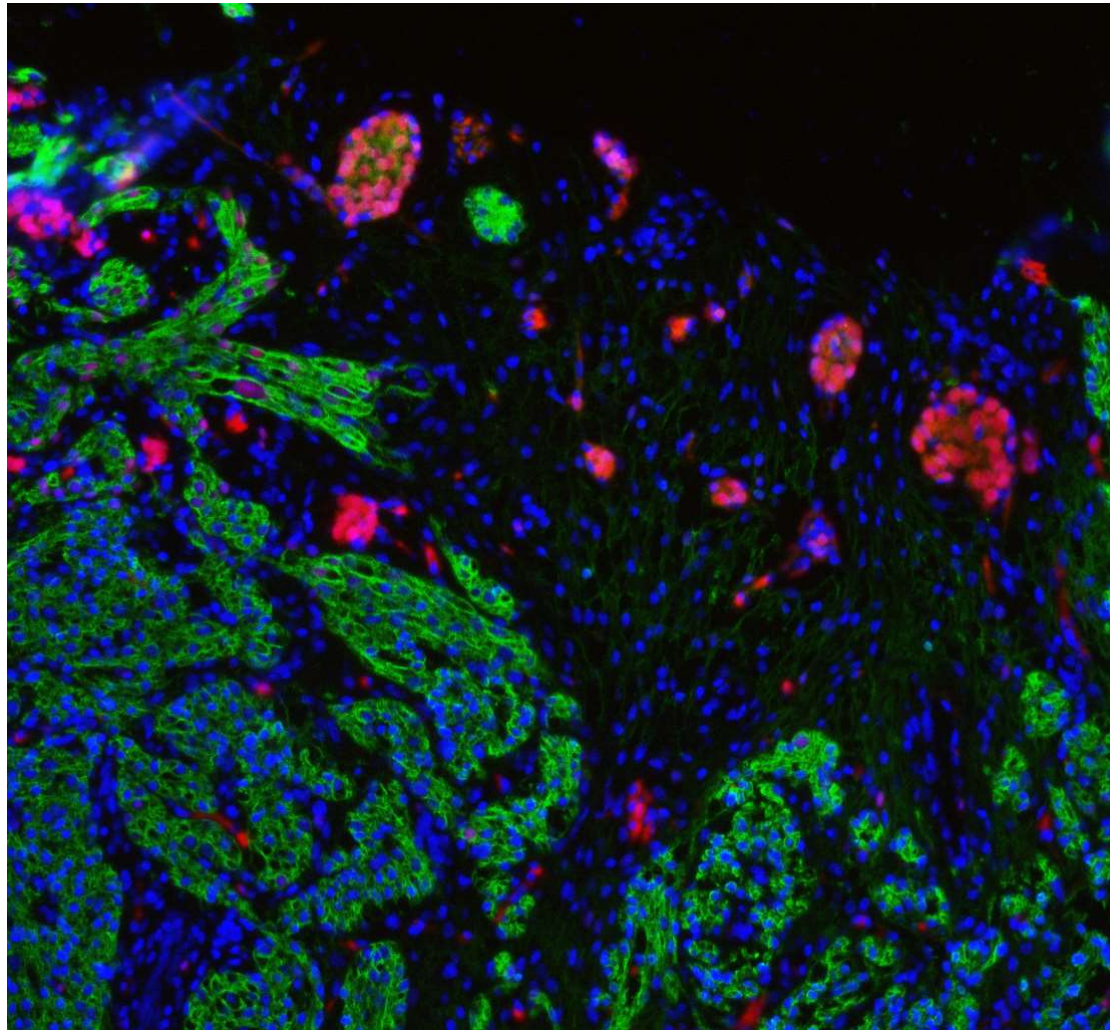
Fluorescent dyes bind to specific cellular structures

- DAPI
- MitoTracker

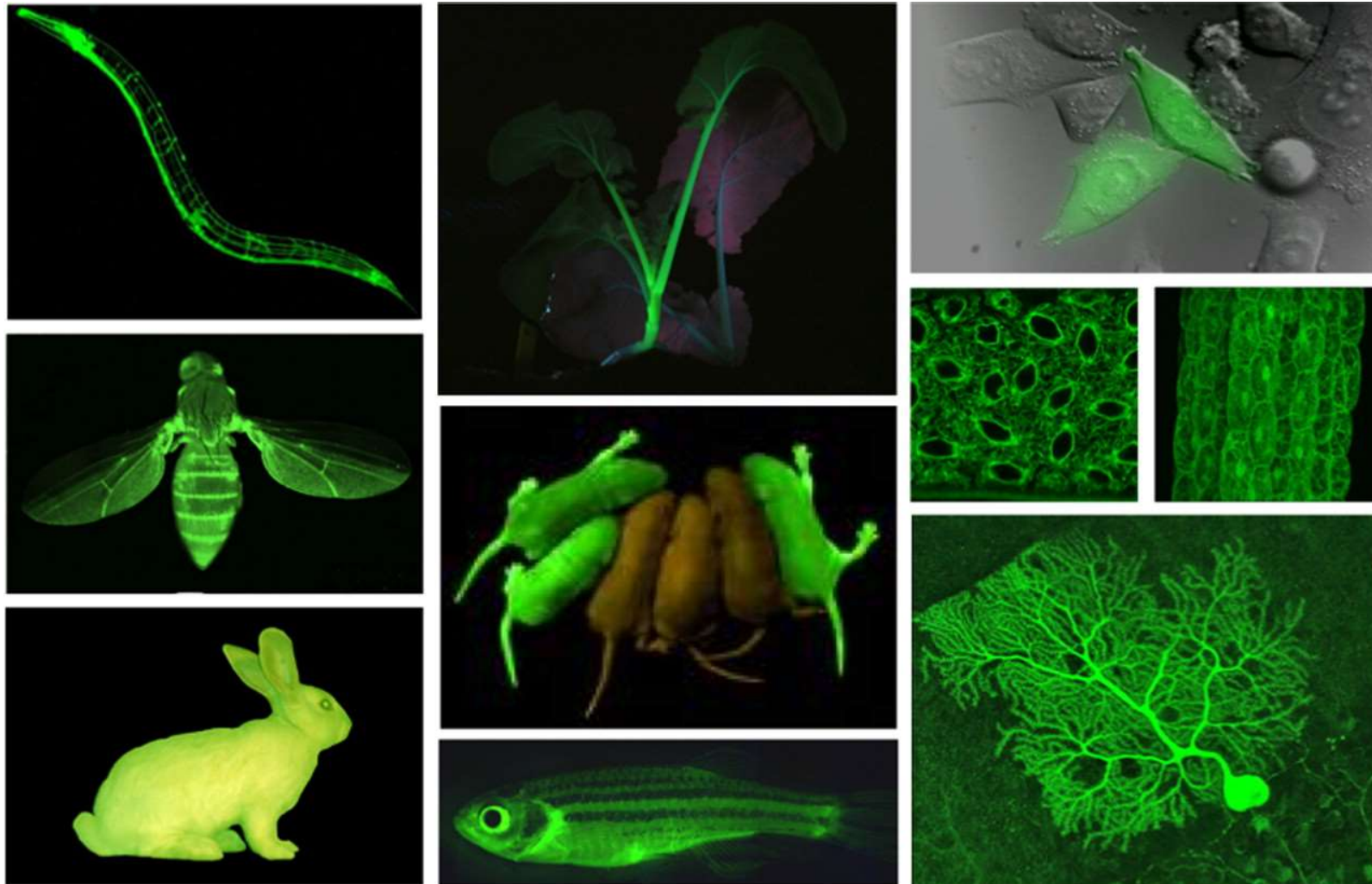


Antibodies conjugated to fluorophores

Stem cell niches



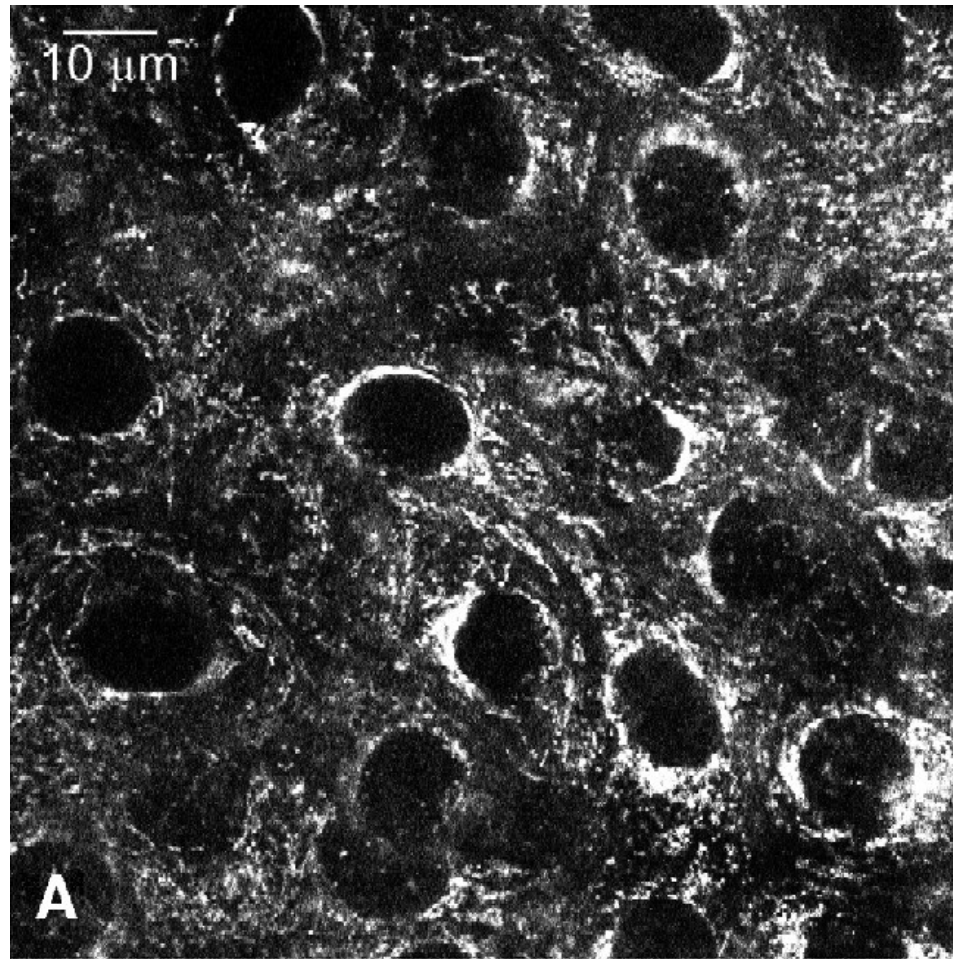
Cells / animals are genetically modified to express GFP



<http://www.pnas.org/content/106/25/10073/F10.expansion.html>

Intrinsic fluorescence

Multiphoton Imaging
Excitation of NADP(H)
 $\lambda_{\text{ex}}=720$ in dermal cells



Limitations of fluorescence microscope

Wide-field

- Thickness of specimens
- No lateral resolution
- Information about colocalization is insufficient
- Use of multiple dyes is limited
- Dyes with similar excitation and emission ranges cannot be discriminated
- Bleaching of fluorophores

Confocal

- Dyes with similar excitation and emission ranges cannot be discriminated
- Simultaneous imaging of several fluorescent probes is limited
- Issues due to autofluorescence within the specimens
- Required time for imaging of thick tissue (several minutes)
- Bleaching of fluorophores
- Quantification of fluorescence signal is limited

Special fluorescence imaging techniques

Fluorescence bleaching

- Fluorescence recovery after photobleaching (FRAP)
- Fluorescence loss in photobleaching (FLIP)
- Fluorescence correlation spectroscopy (FCS)

Quenching

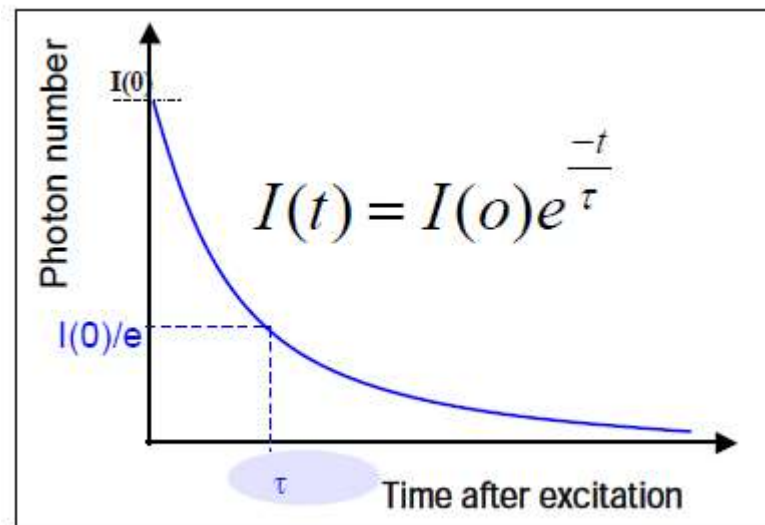
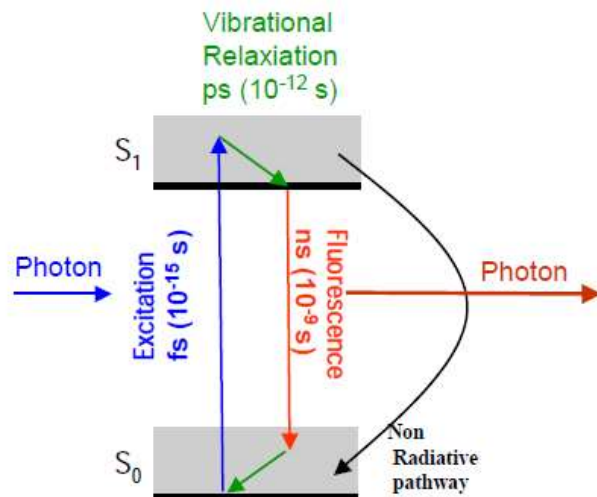
- Förster-Resonance Energy Transfer (FRET)

Fluorescence life-time imaging (FLIM)

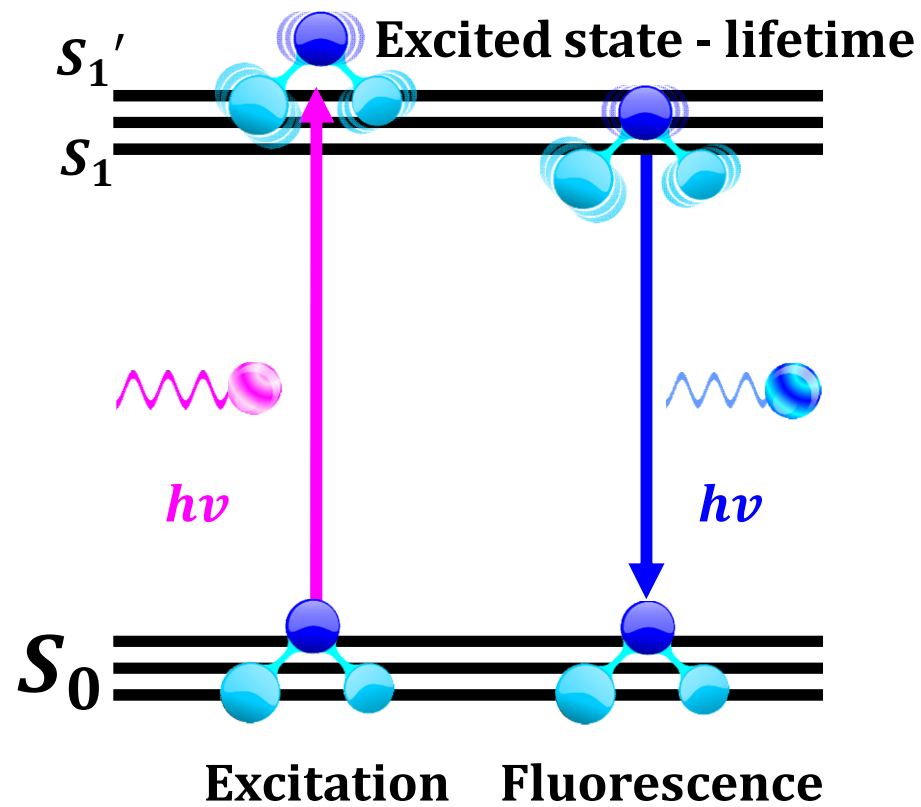
Fluorescence Lifetime Imaging (FLIM)

Fluorescence Life-time Imaging (FLIM)

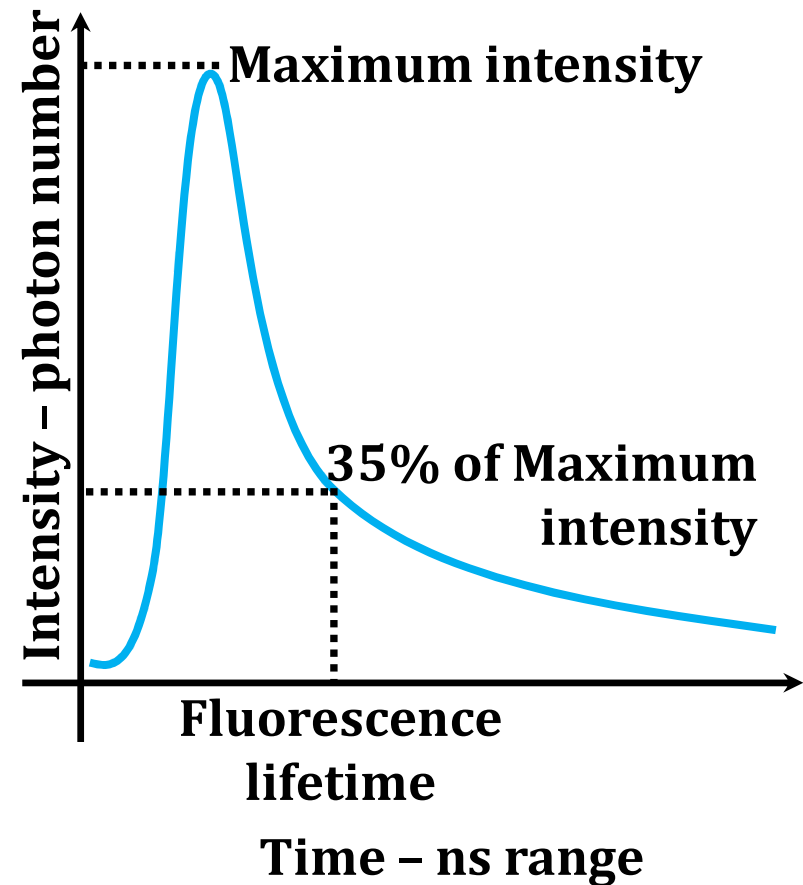
- Every fluorescent molecule has an average time that it spends in the excited state followed after excitation
- This average time is referred as the fluorescent life time τ
- Decay after excitation is an exponential curve
- Fluorescence lifetime imaging uses contrast is based upon the fluorescence lifetimes



Fluorescence lifetime

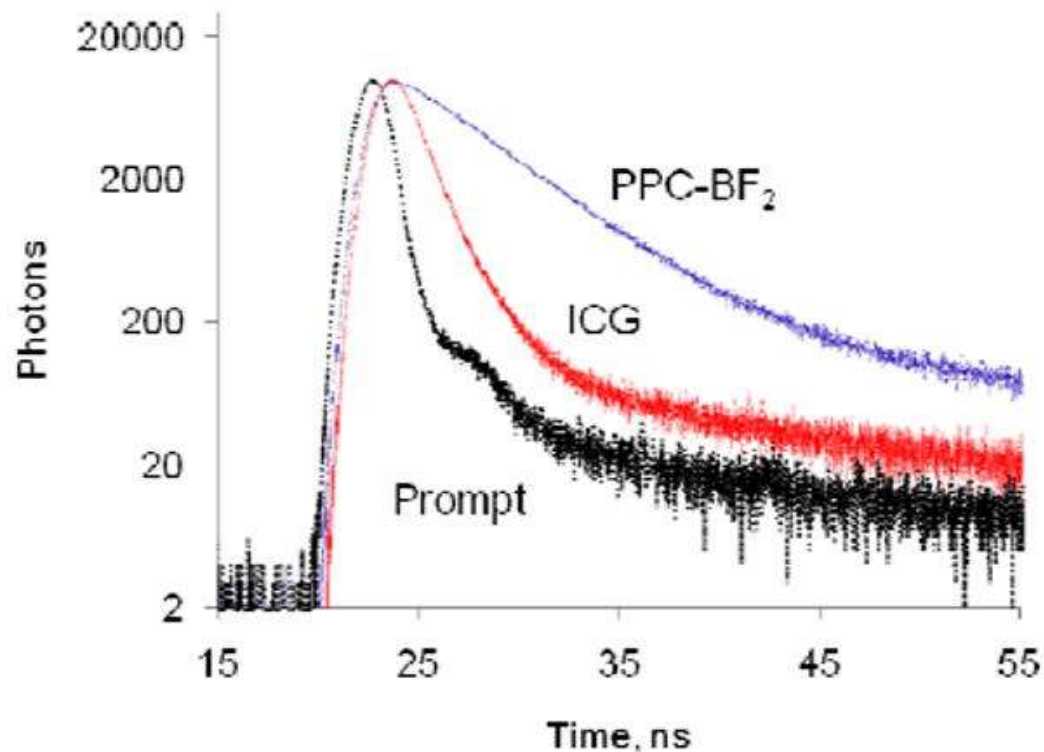


Simplified Jablonski energy diagram



Fluorescence decay curves

- ICG and Pyrrolopyrrole cyanine -BF₂ (PPC) in DMSO
- Excitation at 773 nm and emission at 820 nm
- Prompt corresponds to the instrument response with no fluorophore present

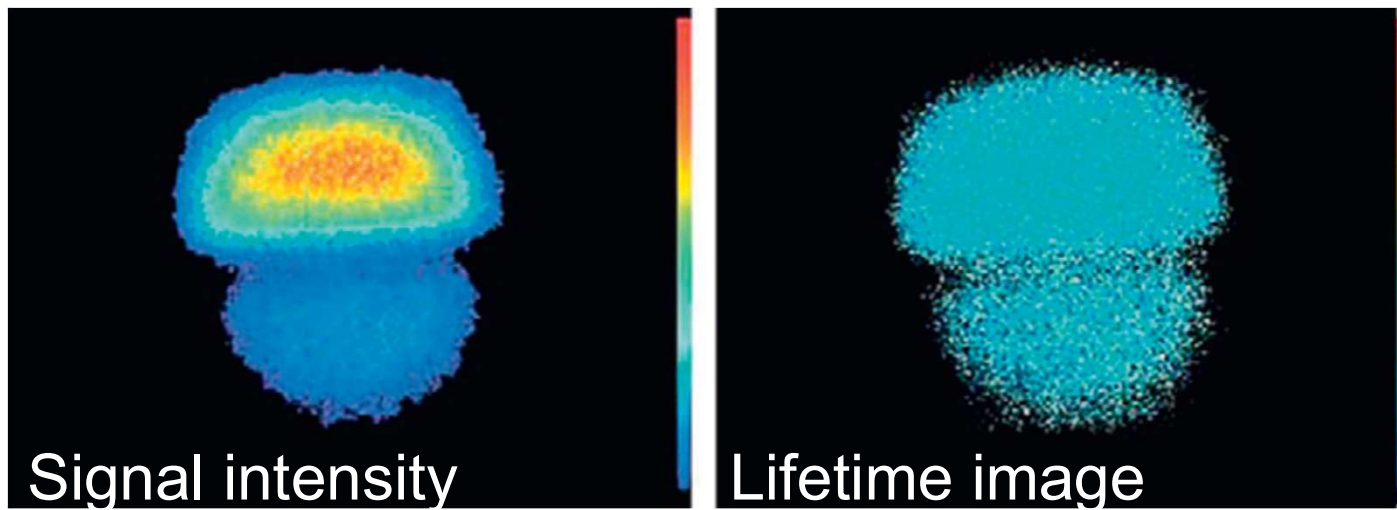


Advantages of FLIM

FLIM is insensitive to a variety of intensity-based artifacts:

- Variations in excitation source intensity
- Detection gain settings
- Optical loss in the optical path
- Sample variation in sample fluorophore concentration
- Photobleaching
- Microscope focusing

Intensity-independent fluorophore lifetimes recovered by FLIM

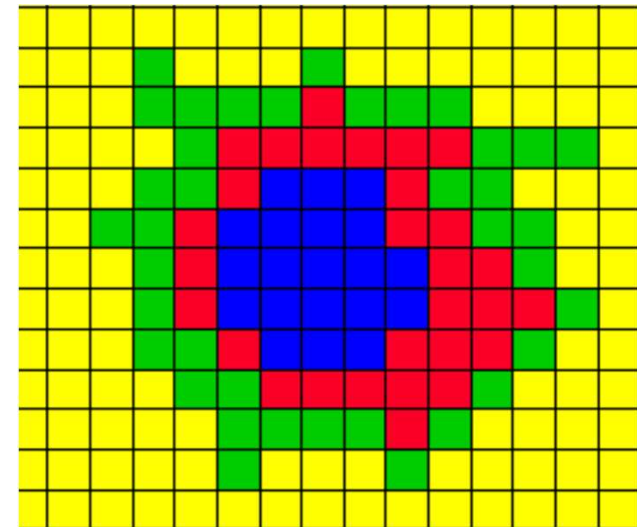


Fluorescence Life-time Imaging (FLIM)

- τ_f is specific for a fluorophore
- Based on τ_f multiple dyes can be distinguished in one channel at high detector sensitivity

FLIM can be used for:

- Ion concentration imaging
- Chemical microenvironment (pH, protein-binding...)
- Quantitative fluorescence measurements



Fluorescence lifetime image

Wavelength -color
lock-up table



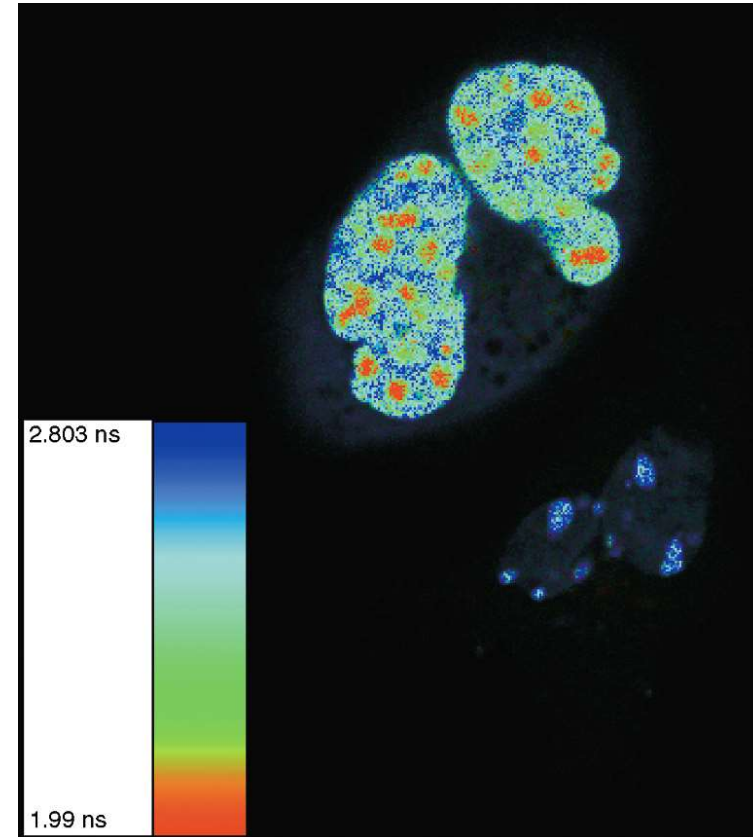
FLIM: Detection modes

Frequency-domain FLIM

- Measurement of the phase shift of fluorescent light with respect to the phase of a modulated excitation source

Time-domain FLIM

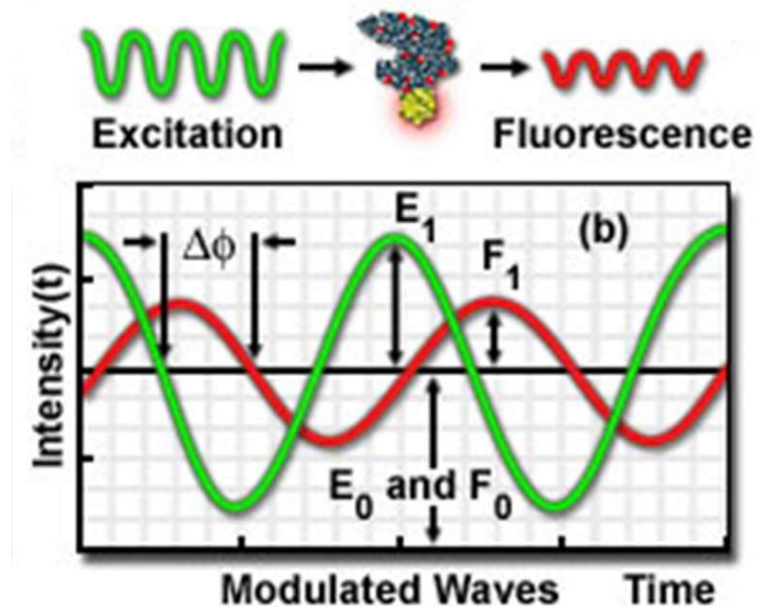
- Measurement of the time dependency of fluorescence intensity with respect to a short excitation pulse.



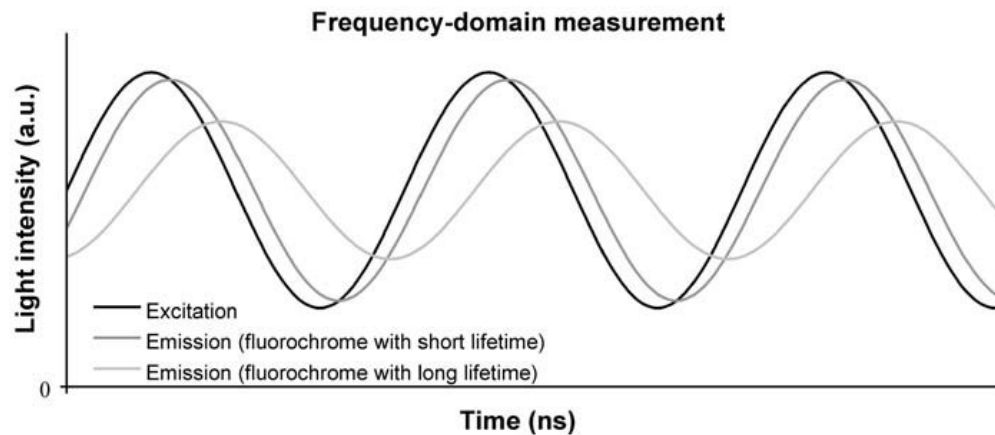
Pawley: Biological confocal microscopy

Frequency-domain FLIM

- Commonly used with wide-field microscopy
- Phase-modulated light source
- Emission is delayed relative to the excitation wave
- Phase shift $\Delta\phi$ is measured



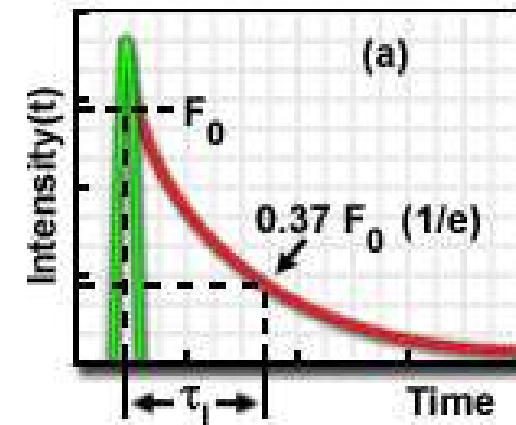
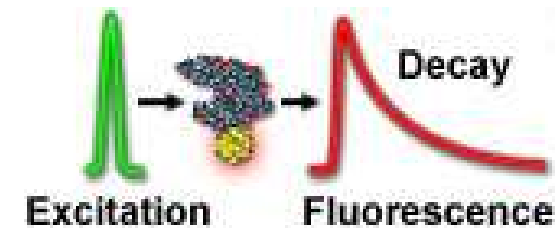
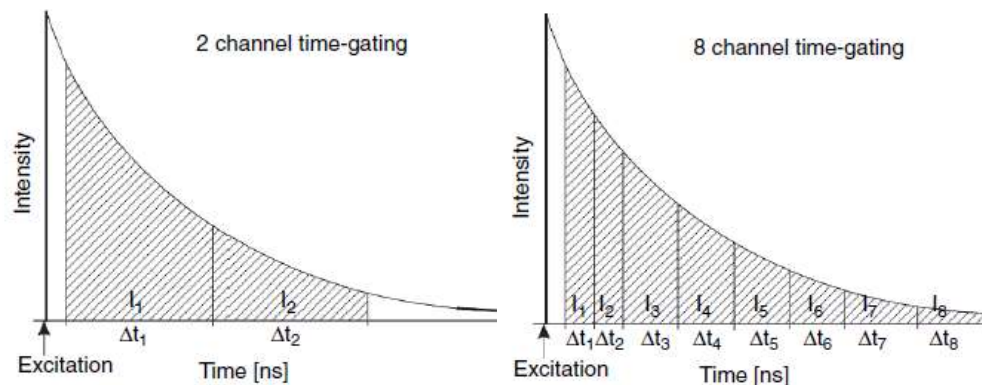
<http://www.olympusfluoview.com/applications/flimintro.html>



Van Munster, 2005

Time-domain FLIM

- Use of a pulsed light source
- Time correlated single photon counting (TCSPC)
- Or time gating



<http://www.olympusfluoview.com/applications/flimintro.html>

Pawley: Biological confocal microscopy

TABLE 27.2. Comparison of Different Lifetime Imaging Methods

	Time Gating	TCSPC	Phase Fluorometry	
			Pulsed	Sinusoidal
Shortest τ_f	0.2–0.5 ns	0.1 ns	0.2–0.5 ns	0.2–0.5 ns
Sensitive to bleaching	No	No	Yes	Yes
Photon economy	Good	Good	Good	Poor
Duty cycle	<0.1	<0.1	<0.1	50%
Acquisition time per pixel	>10 ⁻⁵ s	>10 ⁻⁴ s	>10 ⁻⁵ s	>10 ⁻⁴ s
Costs	Moderate/high	Moderate/high	Moderate/high	Low

Pawley: Biological confocal microscopy

Multi-FLIM Labeling and Segmentation

Determination of six different fluorescent life times by TCSPC

LY = Luciferase Yellow decay times of 4.27 and 4.95 ns

NYO = 2.8 ns

FITC = 3.1 ns

BB = 3.2 ns

Nile Red (NR) = 3.6 ns

Benzopyrylene = 10.8 ns

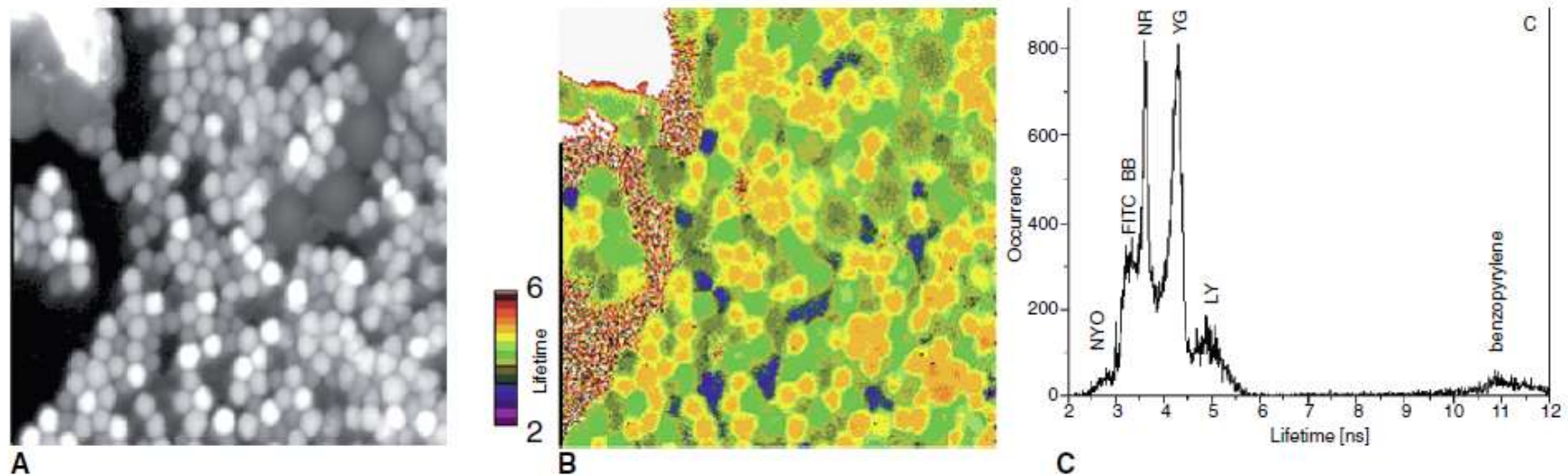
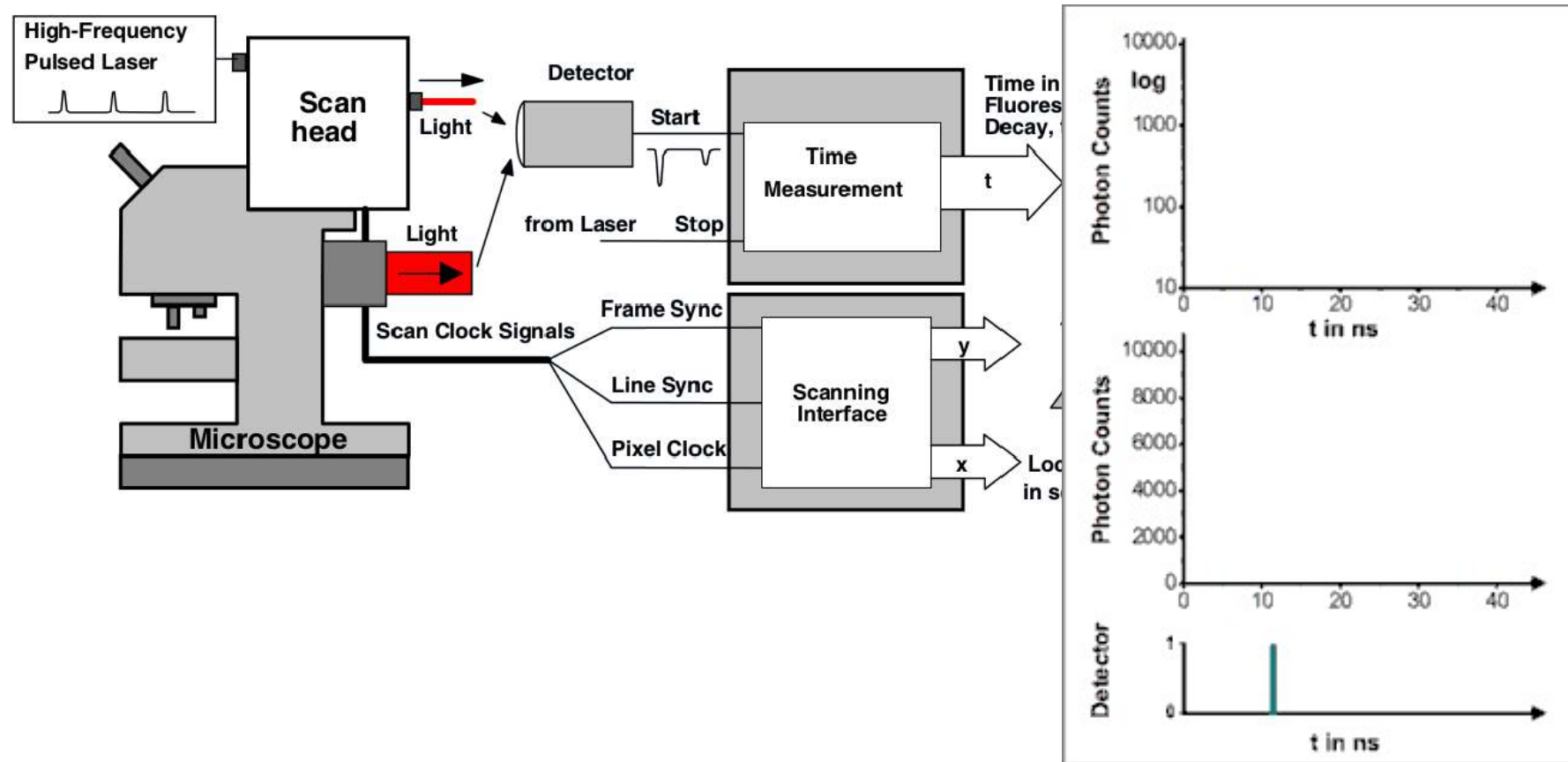


FIGURE 27.8. (A) Intensity image of a specimen containing a number of different fluorescent beads and crystals. (B) Corresponding fluorescence lifetime image. (C) The histogram of fluorescence lifetimes.

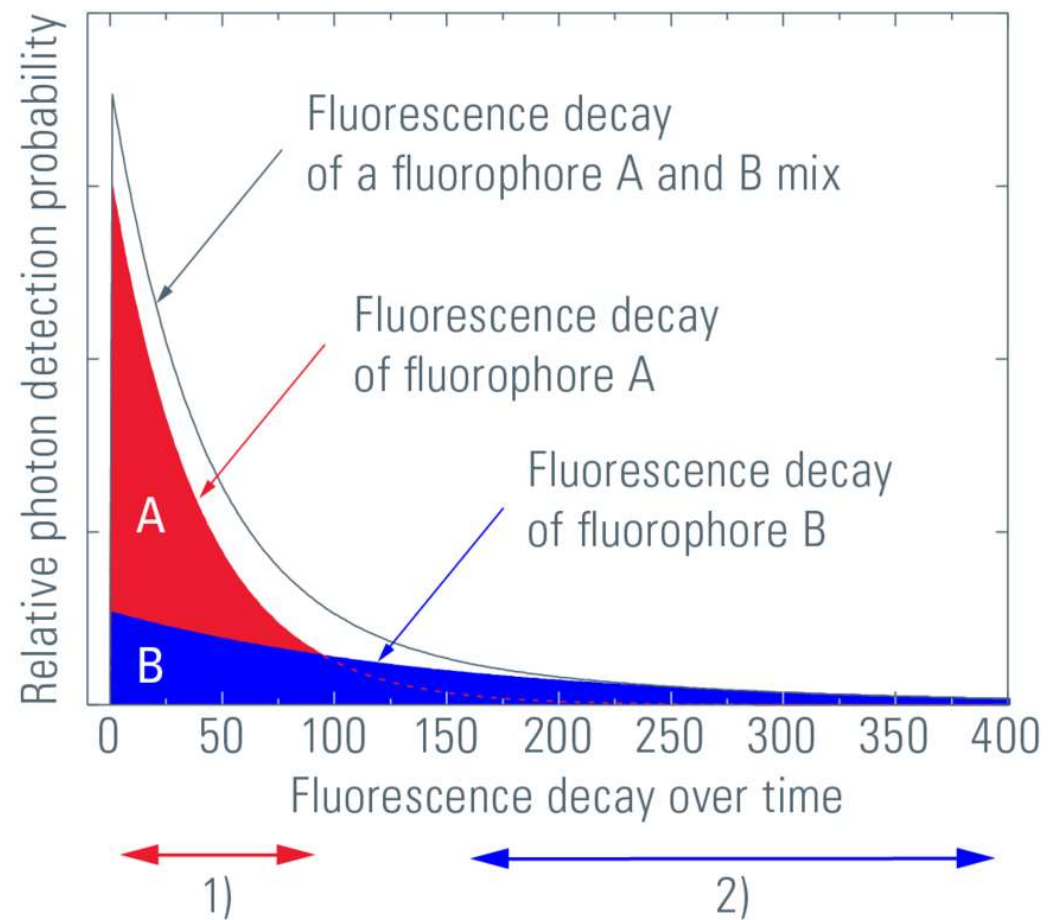
Fluorescence lifetime imaging microscopy (FLIM)



Becker, Wolfgang: The bh TCSPC handbook. 6th. Becker & Hickl GmbH, 2015

Time-domain FLIM

A



Fluorescence lifetime imaging microscopy (FLIM)

Fluorophore	Solvent	Excitation max [nm]	Emission max [nm]	Lifetime [ns]
Endogenous				
Tryptophan	Water	295	353	3.1
Tyrosine	Water	275	304	3.6
Phenylalanine	Water	260	282	6.8
NADH	Water	350	460	0.4
FAD	Water	450	525	4.7
FMN	Water	450	525	2.3
Exogenous				
ATT0 565	Water	561	585	3.4
Rhodamine B	Water	562	583	1.68
Cy3	PBS	548	562	0.3
Cy5	PBS	646	664	1
DAPI	TRIS/EDTA	341	496	0.16
FITC	PB pH 7.8	494	518	4.1
Fluorescein	PB pH 7.5	495	517	4
GFP	Buffer pH 8	498	516	3.2
Hoechst	TRIS/EDTA	336	471	0.35
Lucifer yellow	Water	428	535	5.7

We can excite

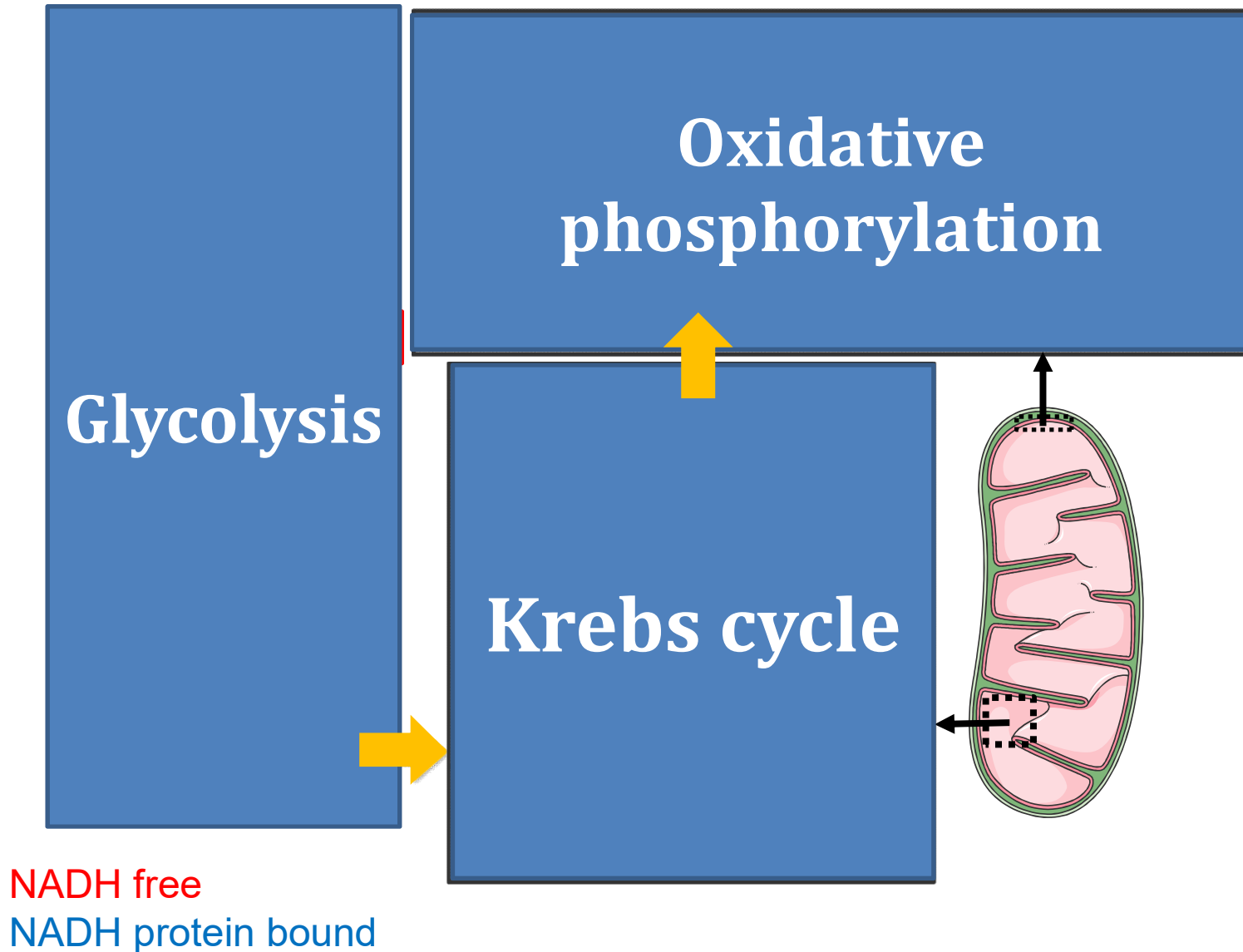
Chen, L.-C., Lloyd 3rd, W. R., Chang, C.-W., Sud, D. & Mycek, M.-A. Fluorescence lifetime imaging microscopy for quantitative biological imaging. *Methods Cell Biol*

Intrinsic Fluorophores

Fluorophore	Excitation λ (nm)	Emission λ (nm)	Fluorescence Lifetime τ (ns)
Keratin		525	
NAD(P)H	340	450–470	0.3–0.6*
Flavins	370, 450	530	5.2
Melanin	UV/VIS	440, 520, 575	0.2/1.9/7.9
Elastin	300–340	420–460	0.2–0.4/0.4–2.5
Collagen	300–340	420–460	0.2–0.4/0.4–2.5
SHG	720–960	360–480	0
Lipofuscin	UV/VIS	570–590	
PPIX	405 ... 630	635, 710	11

Schenke-Layland, J. Biophotonics 2008

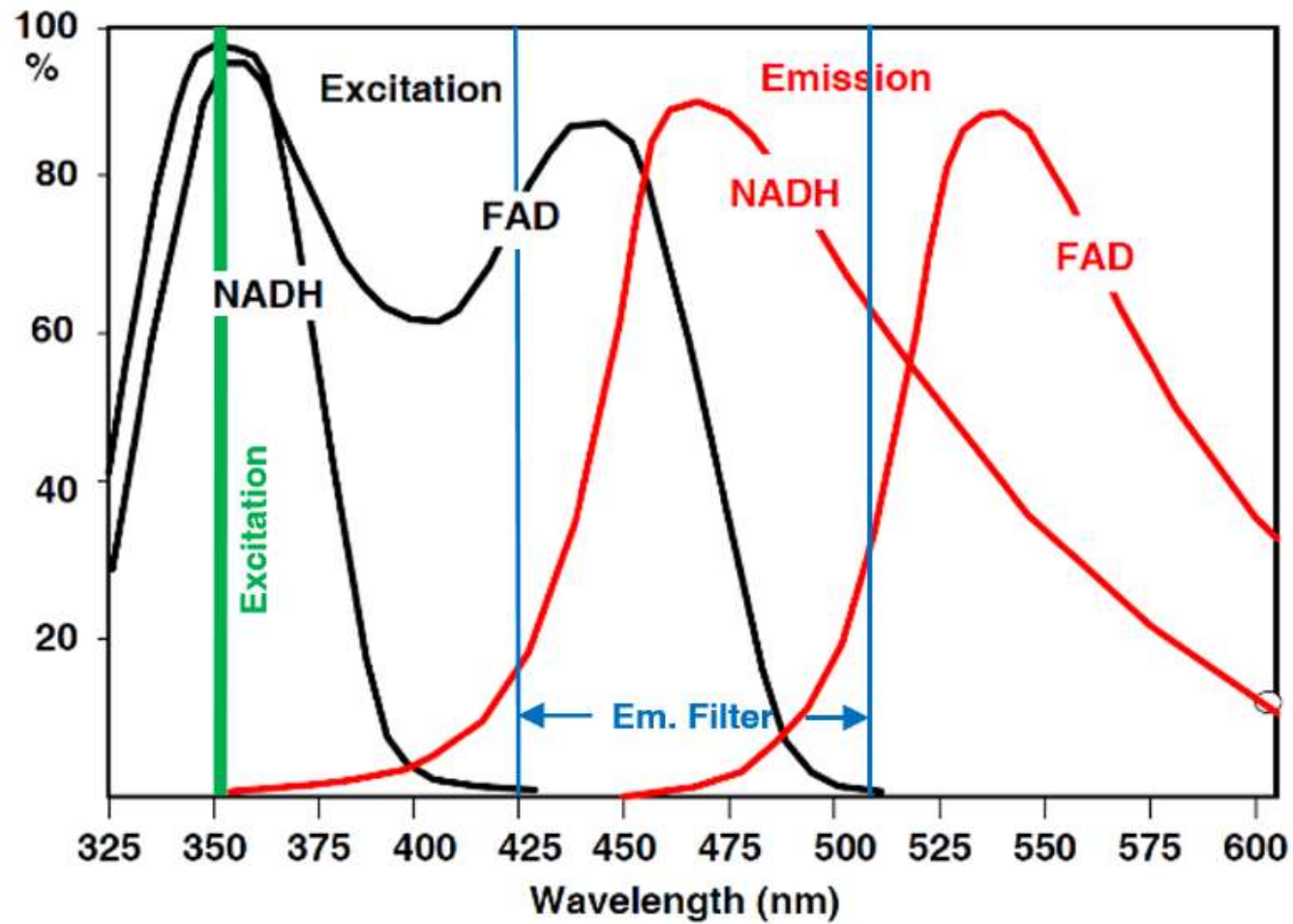
FLIM of NADH – ATP production



NAD(P)H

- Reduced Nicotinamide adenine dinucleotide (phosphate)
- Important cofactor in cell metabolism
- Free NAD(P)H: short lifetime τ_1
- Protein-bound NAD(P)H: long lifetime τ_2
- Typical values: $\tau_1 \sim 700$ ps and $\tau_2 \sim 2600$ ps
- Hypothesis: lifetime and contribution changes with disease

FLIM of NADH



Becker, Wolfgang: The bh TCSPC handbook. 6th. Becker & Hickl GmbH, 2015

For NAD(P)H:

$$F(t) = \alpha_1 \exp\left(-\frac{t}{\tau_1}\right) + \alpha_2 \exp\left(-\frac{t}{\tau_2}\right)$$
$$\tau_m = \alpha_1 \tau_1 + \alpha_2 \tau_2$$

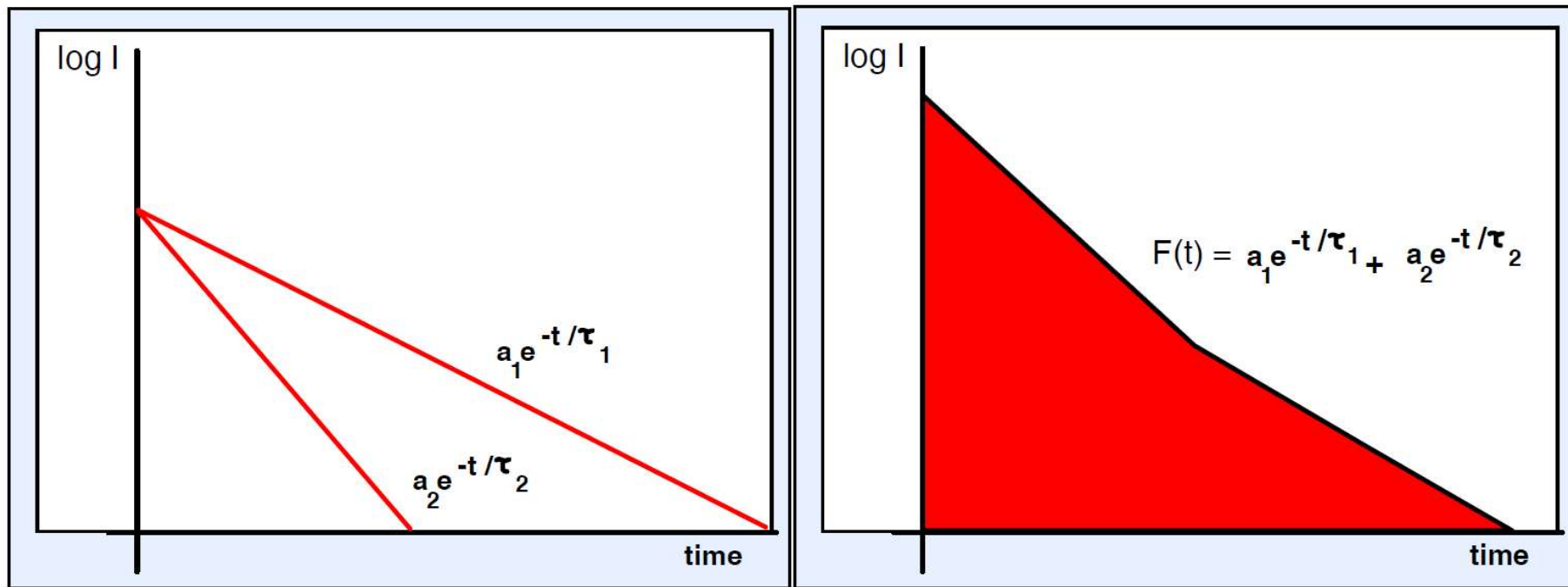
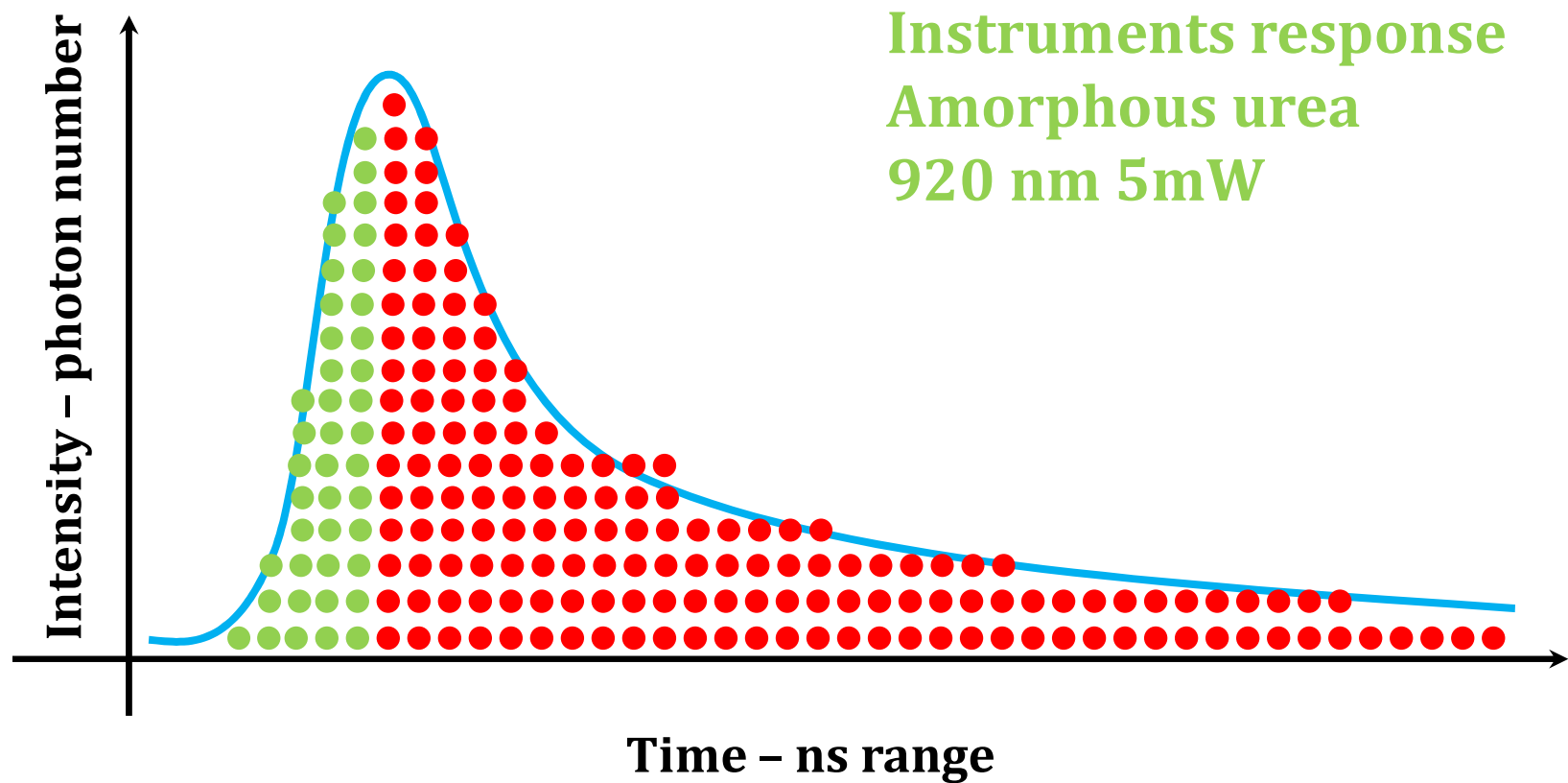


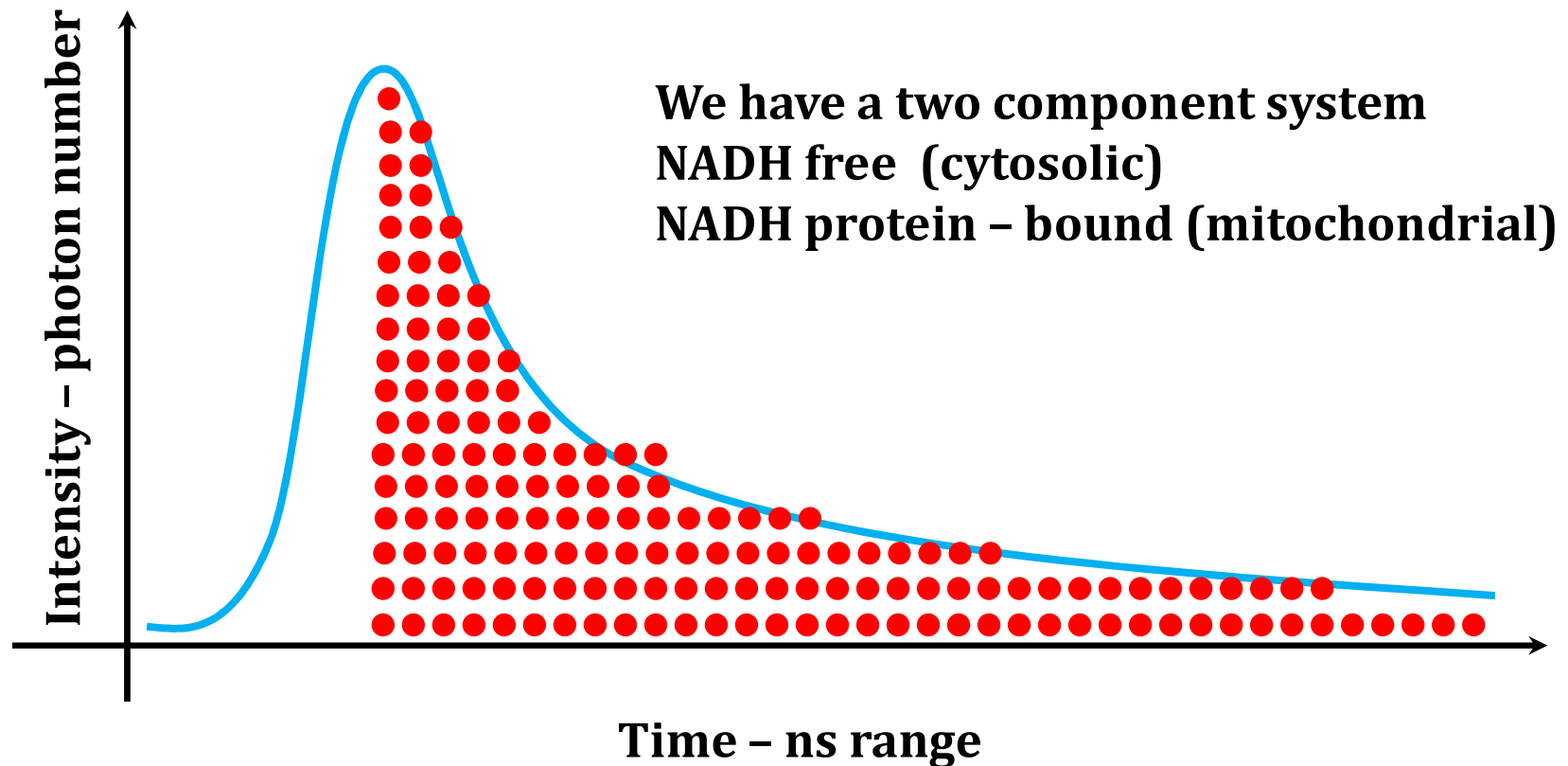
Figure 1: Sum of two exponential decays showing different lifetimes

Source: SPCImage 5.0 manual

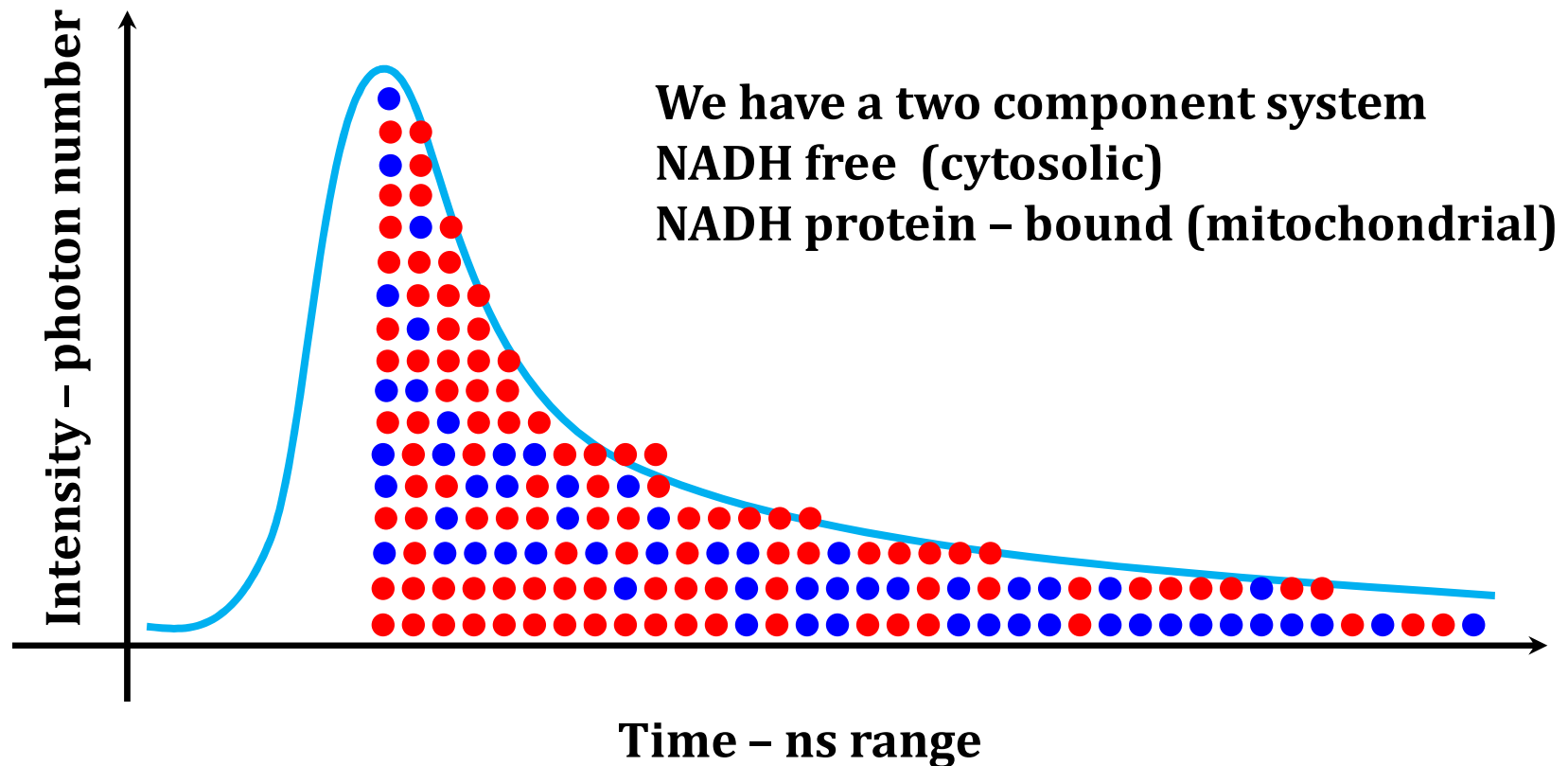
Multiexponential decay fitting



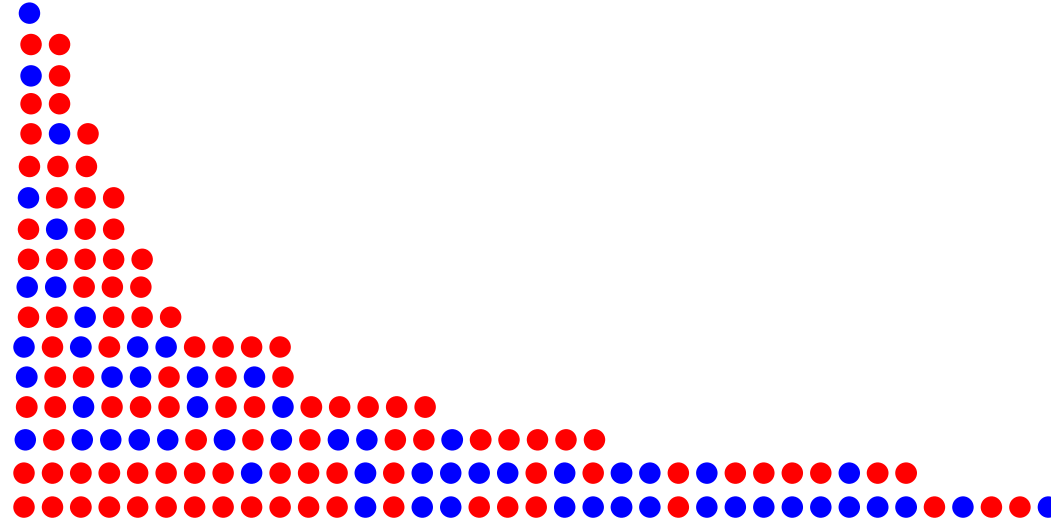
Multiexponential decay fitting



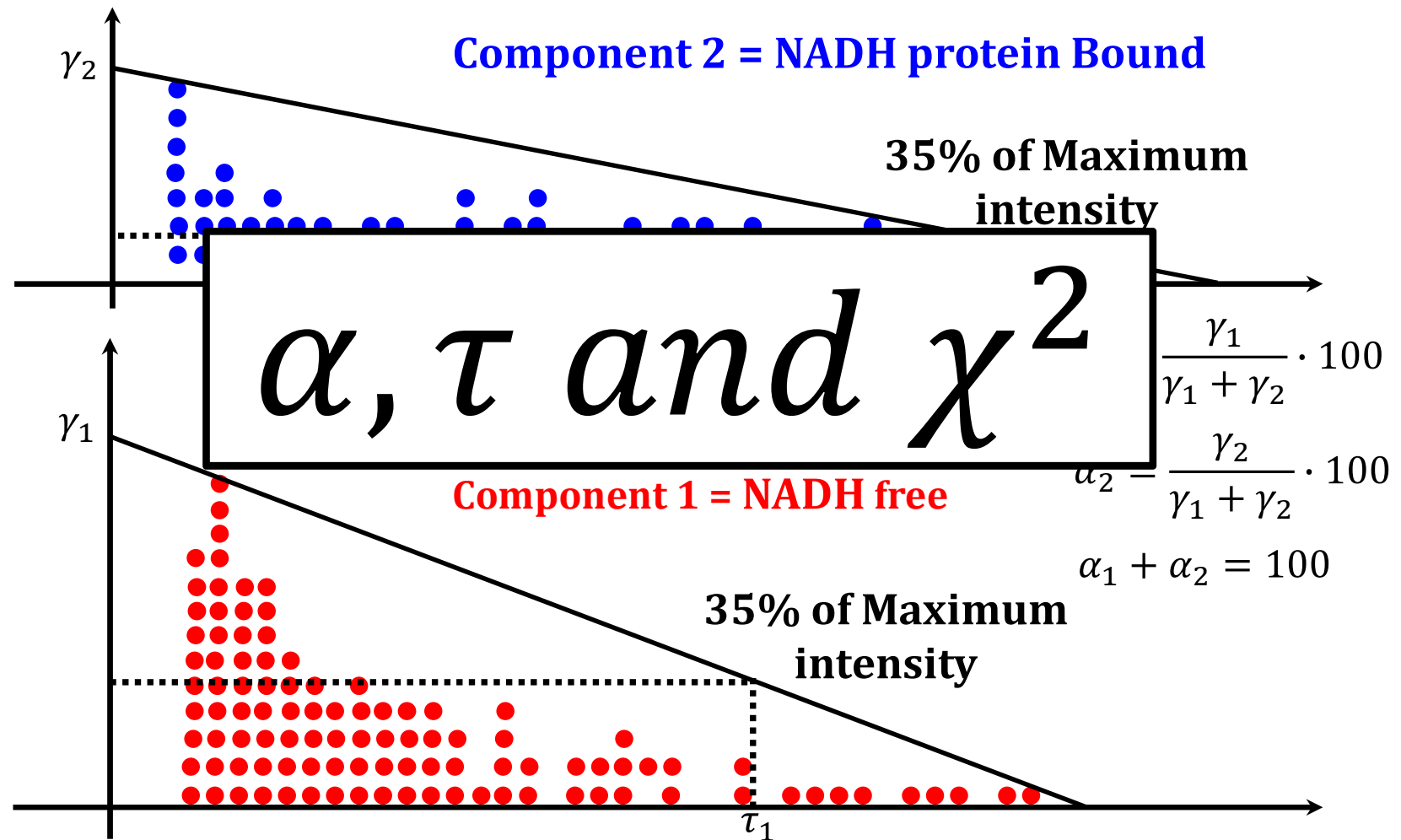
Multiexponential decay fitting



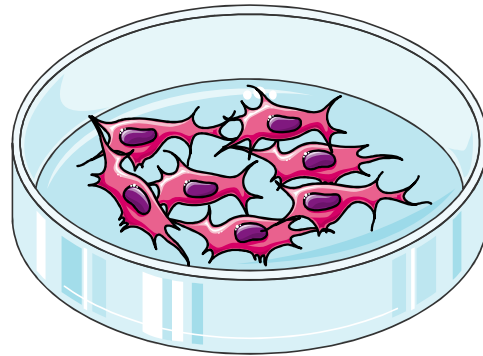
Multieponential decay fitting



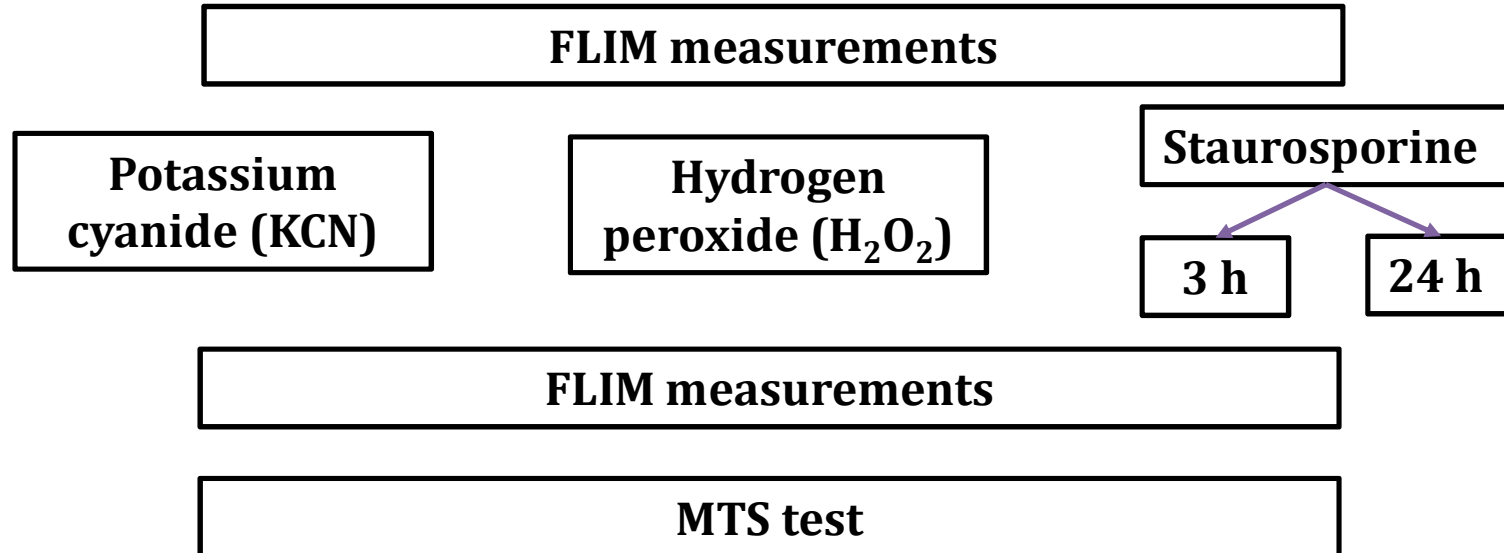
Multieponential decay fitting

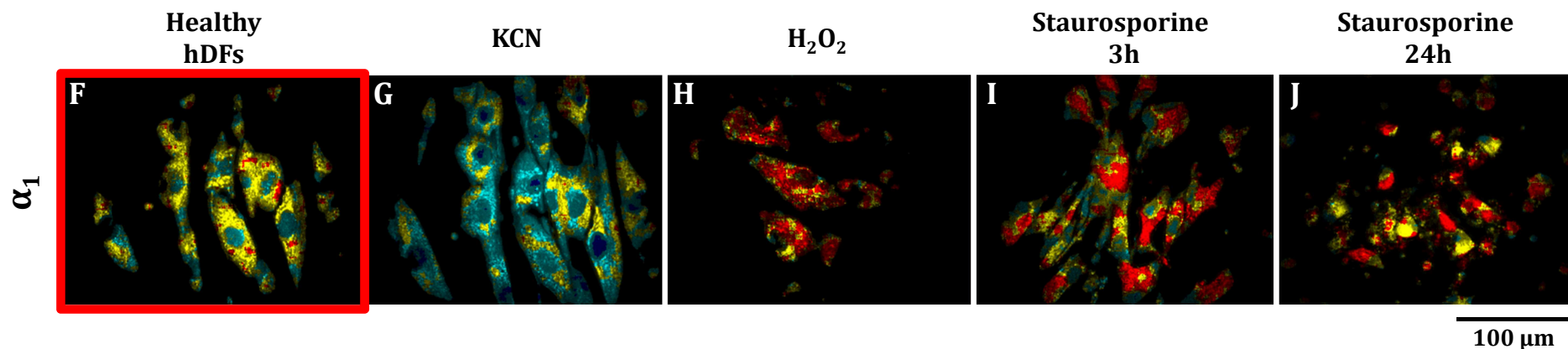


Experimental setup

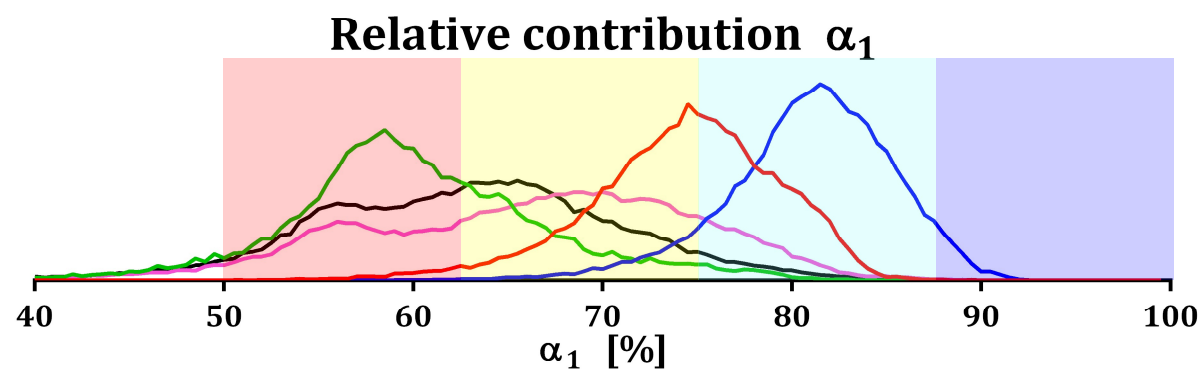


**Human dermal
fibroblast (hDFs)**





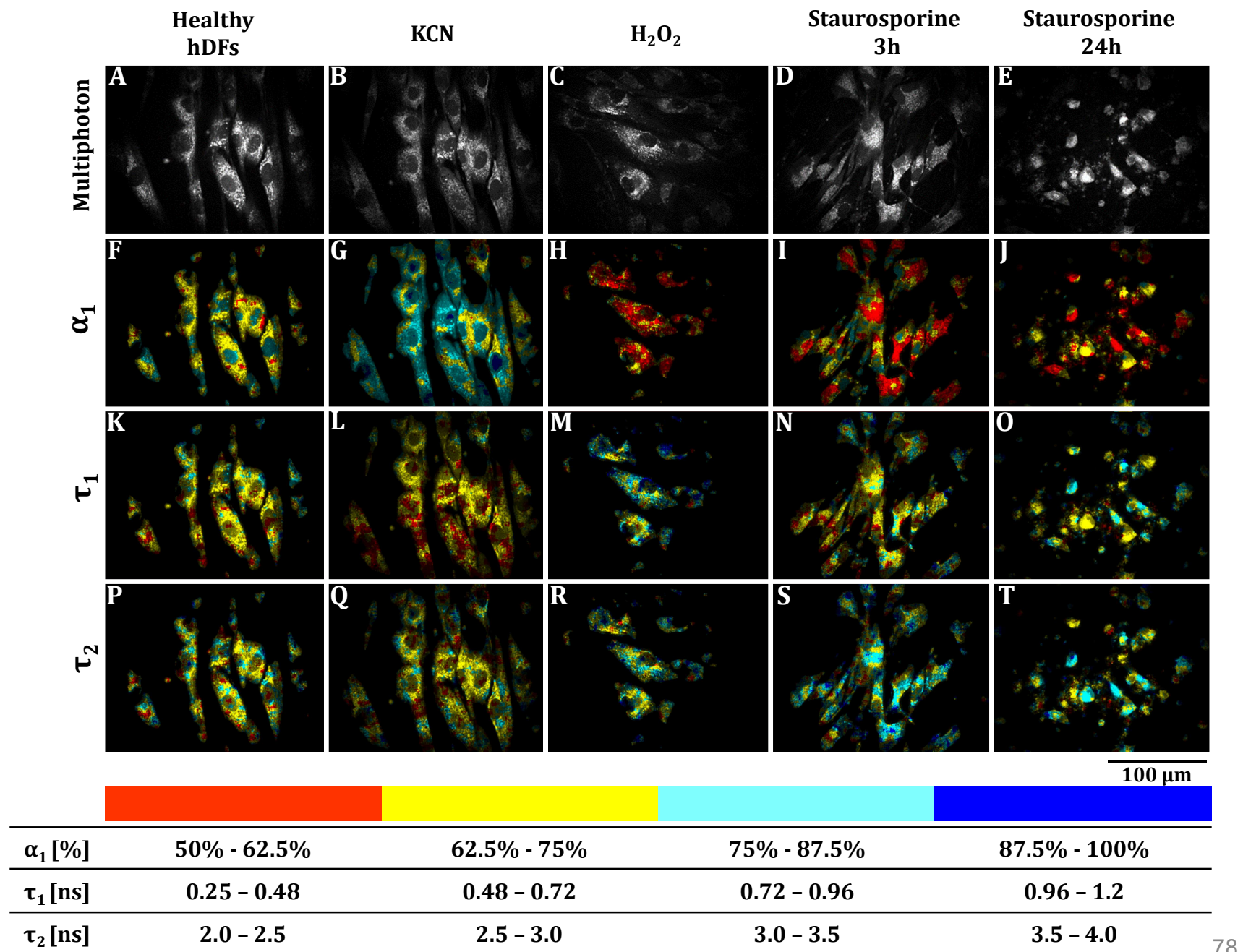
	2.80%	52.75%	44.33%	0.06%
α_1 [%]	50% - 62.5%	62.5% - 75%	75% - 87.5%	87.5% - 100%



Fluorescence lifetime τ_1

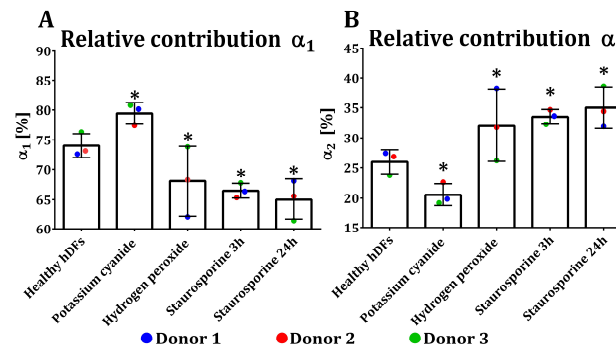
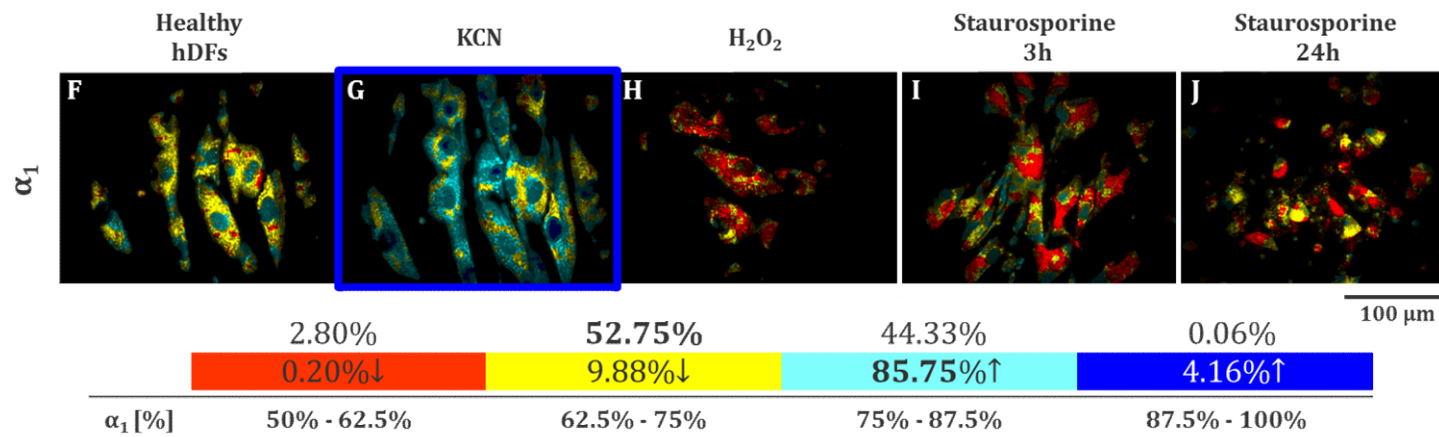
— Healthy hDFs — Potassium cyanide — Hydrogen peroxide

— Staurosporine 3h — Staurosporine 24h



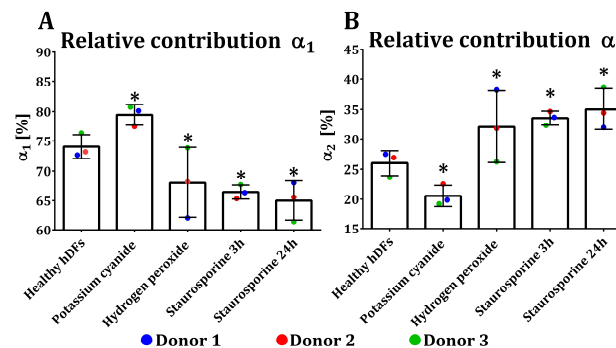
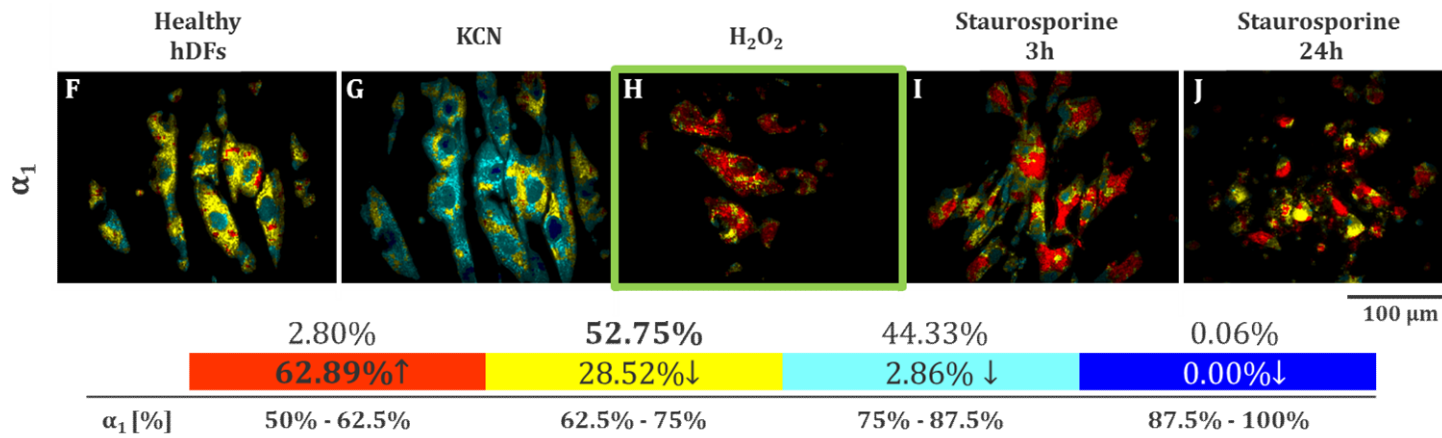
FLIM parameters enable the metabolic evaluation of the inquired specimen

- Oxidative phosphorylation inhibition translates into an increment on the relative contribution of free NADH.



FLIM parameters enable the metabolic evaluation of the inquired specimen

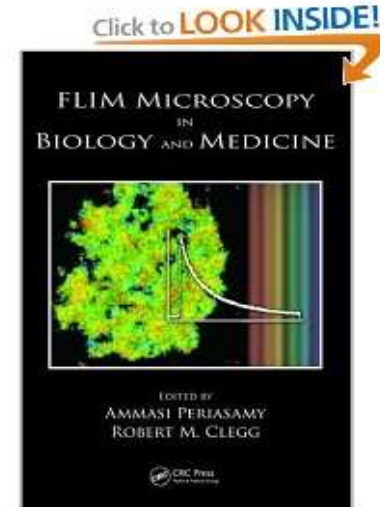
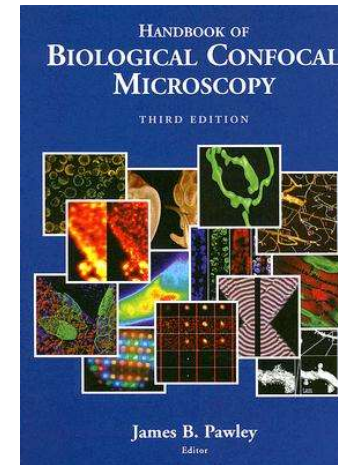
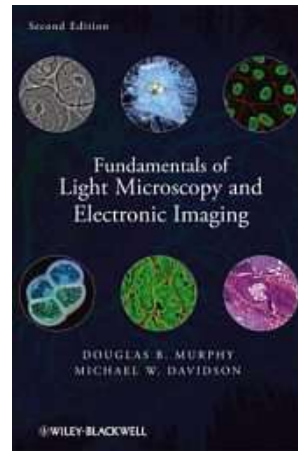
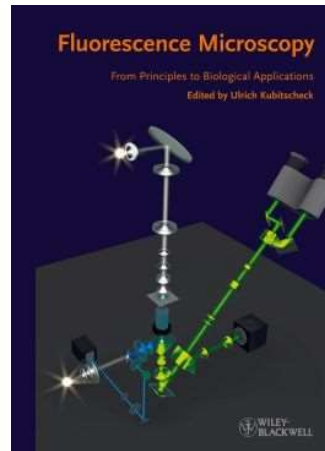
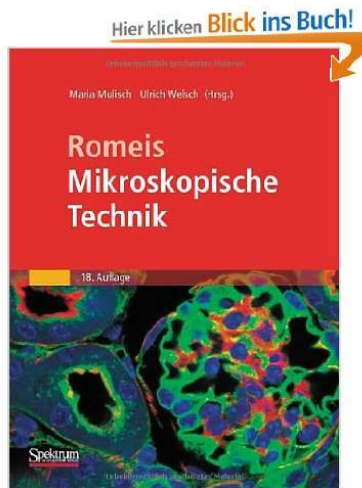
- Glycolysis inhibition results in a reduction of the relative contribution of free NADH.



Summary FLIM

- Intensity-independent information from fluorescent molecules
- Imaging of protein-bound and free metabolites
 - > Label-free Metabolic profiling of cells
- Sensitive to the fluorophores microenvironment
 - > new ways for life scientists to detect, visualize, and investigate structure and function in biological systems

Literature Books



- Romeis: Mikroskopische Technik, ISBN: 978-3-8274-1676-6
- Kubitscheck: Fluorescence Microscopy: From Principles to Biological Applications, Print ISBN: 9783527329229
- Murphy: Fundamentals of Light Microscopy and Electronic Imaging, ISBN Print ISBN: 9780471692140
- Pawley: Handbook Of Biological Confocal Microscopy, ISBN 978-0-387-45524-2
- Periasamy: FLIM microscopy in medicine and biology, ISBN: 978-1420078909